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Abstract: Chitosan (CS)/DNA complex nanoparticles (NPs) have been considered as a vector for gene delivery. Although advantageous for DNA packing and protection, CS-based complexes may lead to difficulties in DNA release once arriving at the site of action. In this study, a new approach through modifying their internal structure by incorporating a negatively charged poly( $\gamma$ -glutamic acid) ( $\gamma$ -PGA) in CS/DNA complexes (CS/DNA/ $\gamma$ -PGA NPs) is reported. The analysis of small angle X-ray scattering results revealed that DNA and  $\gamma$ -PGA formed complexes with CS separately to yield two types of domains, leading to the formation of "compounded NPs". With this unique internal structure, the compounded NPs might disintegrate into a number of even smaller sub-particles after cellular internalization, thus improving the dissociation capacity of CS and DNA. Consequently, after incorporating  $\gamma$ -PGA in CS/DNA complexes, a significant increase in their transfection efficiency was found. Interestingly, in addition to improving the release of DNA intracellularly, the

incorporation of  $\gamma$ -PGA in CS/DNA complexes significantly enhanced their cellular uptake. We further demonstrated that besides a non-specific charged-mediated binding to cell membranes, there were specific trypsin-cleavable proteins involved in the internalization of CS/DNA/ $\gamma$ -PGA NPs. The aforementioned results indicated that  $\gamma$ -PGA played multiple important roles in enhancing the cellular uptake and transfection efficiency of CS/DNA/ $\gamma$ -PGA NPs.

## AUTHOR DECLARATION TEMPLATE

We the undersigned declare that this manuscript is original, has not been published before and is not currently being considered for publication elsewhere.

We wish to draw the attention of the Editor to the following facts which may be considered as potential conflicts of interest and to significant financial contributions to this work. [OR]

We wish to confirm that there are no known conflicts of interest associated with this publication and there has been no significant financial support for this work that could have influenced its outcome.

We confirm that the manuscript has been read and approved by all named authors and that there are no other persons who satisfied the criteria for authorship but are not listed. We further confirm that the order of authors listed in the manuscript has been approved by all of us.

We confirm that we have given due consideration to the protection of intellectual property associated with this work and that there are no impediments to publication, including the timing of publication, with respect to intellectual property. In so doing we confirm that we have followed the regulations of our institutions concerning intellectual property.

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Signed by all authors as follows:

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October 3, 2008

Professor D. F. Williams  
Editor-in-Chief  
*Biomaterials*

Dear Professor Williams:

Attached please find a manuscript entitled "Effects of incorporation of poly( $\gamma$ -glutamic acid) in chitosan/DNA complex nanoparticles on enhancing their cellular uptake and transfection efficiency". The manuscript is intended to be published in *Biomaterials*. It has been solely submitted to *Biomaterials* and that it is not concurrently under consideration for publication in any other journal. We believe these results are of very broad significance and hope you will consider reviewing the manuscript. We value you and the reviewers' suggestions and comments.

Sincerely yours,

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**Impact Statement:**

Chitosan (CS)/DNA complex nanoparticles (NPs) have been considered as a vector for gene delivery; however, CS-based complexes may lead to difficulties in DNA release once arriving at the site of action. In this study, a new approach through modifying their internal structure by incorporating a negatively charged poly( $\gamma$ -glutamic acid) ( $\gamma$ -PGA) in CS/DNA complexes is reported. We demonstrated that DNA and  $\gamma$ -PGA formed complexes with CS separately to yield two types of domains, leading to the formation of "compounded NPs". With this unique internal structure, the compounded NPs might disintegrate into a number of even smaller sub-particles after cellular internalization, thus improving the dissociation capacity of CS and DNA. Interestingly, in addition to improving the release of DNA intracellularly, the incorporation of  $\gamma$ -PGA in CS/DNA NPs significantly enhanced their cellular uptake. Taken together,  $\gamma$ -PGA significantly enhanced the transfection efficiency of this newly developed gene-delivery system.

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**Effects of incorporation of poly( $\gamma$ -glutamic acid) in chitosan/DNA complex nanoparticles on enhancing their cellular uptake and transfection efficiency**

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**Abstract**

Chitosan (CS)/DNA complex nanoparticles (NPs) have been considered as a vector for gene delivery. Although advantageous for DNA packing and protection, CS-based complexes may lead to difficulties in DNA release once arriving at the site of action. In this study, a new approach through modifying their internal structure by incorporating a negatively charged poly( $\gamma$ -glutamic acid) ( $\gamma$ -PGA) in CS/DNA complexes (CS/DNA/ $\gamma$ -PGA NPs) is reported. The analysis of small angle X-ray scattering results revealed that DNA and  $\gamma$ -PGA formed complexes with CS separately to yield two types of domains, leading to the formation of “compounded NPs”. With this unique internal structure, the compounded NPs might disintegrate into a number of even smaller sub-particles after cellular internalization, thus improving the dissociation capacity of CS and DNA. Consequently, after incorporating  $\gamma$ -PGA in CS/DNA complexes, a significant increase in their transfection efficiency was found. Interestingly, in addition to improving the release of DNA intracellularly, the incorporation of  $\gamma$ -PGA in CS/DNA complexes significantly enhanced their cellular uptake. We further demonstrated that besides a non-specific charged-mediated binding to cell membranes, there were specific trypsin-cleavable proteins involved in the internalization of CS/DNA/ $\gamma$ -PGA NPs. The aforementioned results indicated that  $\gamma$ -PGA played multiple important roles in enhancing the cellular uptake and transfection efficiency of CS/DNA/ $\gamma$ -PGA NPs.

**Keywords:** chitosan; poly( $\gamma$ -glutamic acid); transfection efficiency; cellular uptake

## 1. Introduction

Chitosan (CS), a cationic polysaccharide, is biodegradable, non-toxic and tissue compatible [1–4]. It has the potential to condense anionic DNA into a compact structure through electrostatic interactions and has been considered to be a good candidate as non-viral vectors [5–7]. CS/DNA complexes can be readily prepared to provide an effective protection against DNase [8,9]. CS/DNA complexes generally transfect cells more efficiently than naked DNA but less than commercially available liposome formulations. It has been suggested that the strength of electrostatic interactions between CS and DNA prevent their dissociation within cells, thus precluding transcription of DNA and resulting in low transfection [10].

To improve the transfection efficiency of CS/DNA complexes, recent studies have examined the use of low molecular weight CS [8] and developed alternative methods of DNA packaging, adsorption and encapsulation [11]. It has been shown that DNA adsorbed onto the surface of CS/alginate nanoparticles (NPs) reveals a significant improvement in transfection efficiency [10]. However, surface presentation of DNA may render it susceptible to enzymatic degradation. Therefore, an ideal gene delivery system should provide an adequate protection of loaded DNA in the course of delivery and release it when appropriately.

In this study, a new approach for the enhancement of cellular uptake and transfection efficiency of CS/DNA complexes through modifying their internal structure by incorporating a negatively charged poly( $\gamma$ -glutamic acid) ( $\gamma$ -PGA) is reported. We demonstrated that mixing CS, DNA and  $\gamma$ -PGA in aqueous media led to the formation of “compounded NPs” containing domains of CS/DNA and CS/ $\gamma$ -PGA complexes. With this unique internal structure, the compounded NPs might produce a number of even smaller CS/DNA complex NPs after disintegration within cells, thus enhancing the dissociation capacity of CS and DNA due to a large specific surface area (i.e., surface area per unit volume).  $\gamma$ -PGA, a naturally occurring peptide, is water-soluble, biodegradable and non-toxic.  $\gamma$ -PGA-based NPs have been used as a carrier for oral delivery of insulin [12,13] and been employed to deliver protein vaccines and appeared to have a great potential as an adjuvant [14].

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5 The study was to examine characteristics of the compounded NPs containing CS, DNA  
6 and  $\gamma$ -PGA by dynamic light scattering (DLS), transmission electron microscopy (TEM) and  
7 small angle X-ray scattering (SAXS). The potential of gene expression and transfection  
8 efficiency of test NPs was evaluated by fluorescence and luminance spectrometry and flow  
9 cytometry, while their internalization efficiency was examined using a confocal laser  
10 scanning microscope (CLSM) and a flow cytometer.  
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## 18 **2. Materials and Methods**

### 19 *2.1. Plasmid DNA*

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22 The plasmid DNAs used in the study were pEGFP-N2 (4.7 kb, coding an enhanced  
23 green fluorescence protein reporter gene, Clontech, Palo Alto, CA, USA) and pGL4.13 (4.6  
24 kb, coding a firefly luciferase reporter gene, Promega, Madison, WI, USA). pEGFP-N2 and  
25 pGL4.13 were amplified using DH5 $\alpha$  and purified by Qiagen Plasmid Mega Kit (Valencia,  
26 CA, USA) according to the manufacturer's instructions. The purity of plasmids was analyzed  
27 by gel electrophoresis (0.8% agarose), while their concentration was measured by UV  
28 absorption at 260 nm (Jasco, Tokyo, Japan).  
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### 36 *2.2. Preparation of test NPs*

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38 The charge ratio (N/P/C) of test NPs was expressed as the ratio of moles of the amino  
39 groups (N) on CS to the phosphate groups (P) on DNA and the carboxyl groups (C) on  
40  $\gamma$ -PGA. Test NPs at various known N/P/C molar ratios (10/1/0, 10/1/0.5, 10/1/1, 10/1/2,  
41 10/1/4 or 10/1/6) were prepared by an ionic-gelation method. Briefly, an aqueous DNA  
42 (pEGFP-N2 or pGL4.13, 33  $\mu$ g) was mixed with an aqueous  $\gamma$ -PGA (20 kDa, Vedan,  
43 Taichung, Taiwan) at different molar ratios (0, 0.5, 1, 2, 4 or 6) with a final volume of 100  $\mu$ l.  
44 Test NPs were obtained upon addition of the mixed solution, using a pipette, into an aqueous  
45 CS (15 kDa, 0.2  $\mu$ g/ $\mu$ l, 100  $\mu$ l, pH 6.0, Challenge Bioproducts, Taichung, Taiwan) and then  
46 thoroughly mixed for 30–60 s by vortexer and left for at least 1 h at room temperature.  
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### 56 *2.3. Characterization of test NPs*

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58 The encapsulation efficiency of DNA in each studied group was estimated by  
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5 measuring the amount of DNA left in the supernatant after centrifugation [15]. The size  
6 distribution and zeta potential of test NPs were investigated using DLS (Zetasizer 3000HS,  
7 Malvern Instruments Ltd., Worcestershire, UK). The morphology of test NPs was examined  
8 by TEM (JEOL, Tokyo, Japan) [16]. The retardation of DNA in NPs prepared at various  
9 N/P/C ratios was evaluated by electrophoresis.

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11 The internal structure of test NPs was probed by SAXS. Aqueous suspensions of NPs  
12 were directly introduced into the sample cell comprising two ultralene windows for SAXS  
13 measurements. SAXS experiments were performed using a Bruker NanoSTAR SAXS  
14 instrument, which consisted of a Kristalloflex K760 1.5 kW X-ray generator (operated at 40  
15 kV and 35 mA), cross-coupled Göbel mirrors for CuK $\alpha$ -radiation ( $\lambda = 1.54 \text{ \AA}$ ) resulting in a  
16 parallel beam of about  $0.05 \text{ mm}^2$  in cross section at the sample position and a Siemens  
17 multiwire type area detector with 1024 x 1024 resolution mode. All data were corrected by  
18 the empty beam scattering and the sensitivity of each pixel of the area detector. The area  
19 scattering pattern had been circularly averaged to increase the efficiency of data collection.  
20 The intensity profile was output as the plot of the scattering intensity (I) vs. the scattering  
21 vector,  $q = 4\pi/\lambda \sin (\theta/2)$  ( $\theta =$  scattering angle) [17].

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23 The dissociation of DNA from its carrier within cells was investigated by exposing test  
24 NPs (encapsulated with pGL4.13) in a phosphate buffered saline (PBS) at pH 7.2 and then  
25 treating with restriction enzymes (*Bam*HI and *Hind*III, New England Biolabs, Ipswich, MA,  
26 USA), simulating the pH environments in the cytoplasm and nuclei.

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2.4. *In vitro* transfection

HT1080 (human fibrosarcoma) cells were cultured in DMEM media supplemented with  
2.2 g/l sodium bicarbonate and 10% fetal bovine serum (FBS). Cells were subcultured  
according to ATCC recommendations without using any antibiotic. For transfection, cells  
were seeded on 12-well plates at  $2 \times 10^5$  cells/well and transfected the next day at 50–80%  
confluency. Prior to transfection, the media were removed and cells were rinsed twice with  
transfection media (DMEM without FBS, pH 6.0). Cells were replenished with 0.6 ml  
transfection media containing test NPs or naked DNA at a concentration of 2  $\mu\text{g}$  DNA/well.

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5 At 2 h post transfection, the transfection media containing NPs were removed, the cells  
6 rinsed twice with transfection media and refilled with FBS-containing media until analysis at  
7 48 h after transfection. Cells were then observed under a fluorescence microscope (Carl  
8 Zeiss Optical, Chester, VA, USA) to monitor any morphological changes and to obtain an  
9 estimate of the transfection efficiency. Cells transfected with Lipofectamine<sup>TM</sup> 2000  
10 (Invitrogen, Carlsbad, CA, USA) were used as a positive control and those without any  
11 treatment were used as a negative control. Transfection efficiencies were presented by two  
12 numeric indicators: percentage of cells transfected and gene expression level [18].  
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### 20 *2.5. Percentage of cells transfected*

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22 The percentage of cells transfected was quantitatively assessed at 48 h after transfection  
23 by flow cytometry. Cells were detached by 0.05% collagenase. Cell suspensions were then  
24 transferred to microtubes, fixed by 4% paraformaldehyde and determined the transfection  
25 efficiency by a flow cytometer (Beckman Coulter, Fullerton, CA, USA) equipped with a 488  
26 nm argon laser for excitation. For each sample, 10,000 events were collected and  
27 fluorescence was detected. Signals were amplified in logarithmic mode for fluorescence to  
28 determine the EGFP positive events by a standard gating technique. The percentage of  
29 positive events was calculated as the events within the gate divided by the total number of  
30 events, excluding cell debris.  
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### 40 *2.6. Gene expression level*

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42 The gene expression levels of cells were assayed by quantifying the expressions of  
43 EGFP or luciferase. The expression level of EGFP was quantified by comparing average  
44 fluorescence of  $1 \times 10^6$  cells. Briefly, cells were treated with test NPs encapsulated with  
45 pEGFP-N2 or naked DNA. After 48 h, cells were detached as described in Section 2.5.  
46 Aliquots of 50  $\mu$ l were transferred to 96-well black plates and the fluorescence intensity was  
47 analyzed using a multi-detection microplate reader (Molecular Devices, Sunnyvale, CA,  
48 USA) and normalized to the total cell number of each sample.  
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56 For the expression of luciferase, cells were plated on 24-well plates and transfected as  
57 described in Section 2.4 with the exception that 1  $\mu$ g pGL4.13 was used. The cells  
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5 transfected were lysed by 100  $\mu$ l of passive lysis buffer (Promega). The cell lysate was  
6 transferred into a 1.5-ml microtube, while the cell debris was separated by centrifugation  
7 (14,000 rpm, 5 min). Subsequently, a 100  $\mu$ l of the luciferase assay reagent (Promega) was  
8 added to a 20  $\mu$ l of the supernatant and the relative luminescence of the sample was  
9 determined by a microplate luminometer (Berthold Technologies, Bad Wildbad, Germany)  
10 and normalized to the total cell protein concentration by the Bradford method.  
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### 16 *2.7. Fluorescent NP preparation, CLSM visualization and flow-cytometry analysis*

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Cy3-labeled CS (Cy3-CS) and FITC-labeled CS (FITC-CS) were synthesized as per the methods described in the literature [19,20]. To remove the unconjugated Cy3 and FITC, the synthesized Cy3-CS and FITC-CS were dialyzed in the dark against deionized (DI) water and replaced on a daily basis until no fluorescence was detected in the supernatant. The resultant Cy3-CS and FITC-CS were lyophilized in a freeze dryer. Cy3- and FITC-labeled NPs were then prepared as described in Section 2.2 to track the internalization of NPs by CLSM and to quantify their cellular uptake by flow cytometry, respectively.

To track the internalization of NPs, cells were seeded on 12-well plates with a sterile glass coverslip at  $2 \times 10^5$  cells/well and incubated overnight. Subsequently, cells were rinsed twice with transfection media and transfected with Cy3-labeled NPs. After incubation for 2h, test samples were aspirated. Cells were then washed twice with pre-warmed PBS before they were fixed in 4% paraformaldehyde. Finally, the fixed cells were examined under a CLSM (TCS SL, Leica, Germany).

To quantify the cellular uptake of NPs, cells were plated on 12-well plates and transfected with FITC-labeled NPs at a concentration of 2  $\mu$ g DNA/well for 1 h. After transfection, cells were detached by 0.05% collagenase and transferred to microtubes. Subsequently, cells were resuspended in PBS containing 1mM EDTA and fixed in 4% paraformaldehyde. Finally, the cells were introduced into a flow cytometer equipped with a 488-nm argon laser.

To determine whether cell-surface proteins were involved in the uptake of test NPs, cells were treated with trypsin (0.01%, 0.025% or 0.05% by w/v in Hanks' balanced salt

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5 solution) for 5 min prior to transfection [21]. Cells were then treated with FITC-labeled NPs  
6 and analyzed by flow cytometry as described above.  
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## 8 9 *2.8. MTT assay*

10 The cytotoxicity of NPs was evaluated *in vitro* using the MTT assay [22]. HT1080 cells  
11 were seeded on 24-well plates at  $5 \times 10^4$  cells/well, allowed to adhere overnight and  
12 transfected by test NPs containing 1  $\mu$ g DNA. After 2 h, test samples were aspirated and  
13 cells were incubated for another 46 h. Subsequently, cells were incubated in a growth  
14 medium containing 1 mg/ml MTT reagent for an additional 4 h; a 500  $\mu$ l of dimethyl  
15 sulfoxide was added to each well to ensure solubilization of formazan crystals. Finally, the  
16 optical density readings were performed using a multiwall scanning spectrophotometer  
17 (Dynatech Laboratories, Chantilly, VA, USA) at a wavelength of 570 nm.  
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## 27 *2.9. Statistical analysis*

28 Comparison between groups was analyzed by the one-tailed Student's *t*-test (SPSS,  
29 Chicago, Ill). All data are presented as a mean value with its standard deviation indicated  
30 (mean $\pm$ SD). Differences were considered to be statistically significant when the *P* values  
31 were less than 0.05.  
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# 38 **3. Results**

## 39 *3.1. Agarose gel retardation*

40 The binding capacity of CS with DNA prepared at various N/P ratios was evaluated  
41 using the gel retardation assay and the results are shown in Fig. 1a. The CS/DNA complex  
42 with an N/P ratio of 5/1 was physically unstable, resulting in the partial dissociation of  
43 plasmids. In contrast, as the N/P ratio was increased to 10/1, the migration of DNA was  
44 retarded completely. Therefore, preparation of test NPs was carried out using an N/P ratio of  
45 10/1 in the subsequent experiments. As shown in Fig. 1b, by incorporating  $\gamma$ -PGA in NPs  
46 (N/P/C ratios of 10/1/0.5 to 10/1/6), no significant DNA release was observed.  
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## 56 *3.2. Morphology, size, zeta potential and encapsulation efficiency of test NPs*

57 TEM was used to examine the morphology of test NPs prepared at various N/P/C ratios  
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5 (Fig. 2). As shown, the CS/DNA complex (N/P/C ratio of 10/1/0) had a heterogeneous size  
6 distribution with a donut, rod or pretzel shape. In contrast, with the incorporation of  $\gamma$ -PGA,  
7 test NPs (N/P/C ratios of 10/1/0.5 to 10/1/6) were spherical in shape with a relatively  
8 homogeneous size distribution.  
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12 The size distribution and zeta potential of the prepared NPs in aqueous environment  
13 were investigated by DLS. As shown in Table 1, with an increase in the amount of  $\gamma$ -PGA  
14 incorporated, the size of NPs increased appreciably while their polydispersity index and zeta  
15 potential value decreased noticeably. The diameters of NPs measured by DLS were  
16 relatively larger than those observed by TEM. This is because the diameters of NPs obtained  
17 by DLS reflected their hydrodynamic diameters swelled in aqueous solution, while those  
18 observed by TEM were the diameters of dried NPs. The encapsulation efficiencies of DNA  
19 in NPs prepared at distinct N/P/C ratios were about the same and approached 100%.  
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### 28 3.3. Effects of $\gamma$ -PGA on internal structure of NPs and their release of DNA 29

30 SAXS was used to examine the internal structure of test NPs. Fig. 3a shows the SAXS  
31 profiles of CS/ $\gamma$ -PGA (N/P/C ratio of 10/0/6), CS/DNA (N/P/C ratio of 10/1/0) and  
32 CS/DNA/ $\gamma$ -PGA (N/P/C ratios of 10/1/1 to 10/1/6) NPs. The scattering profile of CS/ $\gamma$ -PGA  
33 NPs displayed a featureless monotonic decay, revealing a disordered internal structure. In  
34 this case, the SAXS intensity might stem from the characteristic concentration fluctuations  
35 of the CS/ $\gamma$ -PGA complex within NPs. The SAXS profile of CS/DNA NPs was found to  
36 display a peak at  $2.8 \text{ nm}^{-1}$  associated with the spatial correlation of DNA in CS/DNA  
37 complexes. The characteristic spacing between DNA calculated from the peak position ( $q_{\text{DNA}}$ )  
38 via  $d_{\text{DNA}} = 2\pi/q_{\text{DNA}}$  was 2.24 nm. Therefore, the DNA chains in CS/DNA complexes were  
39 packed densely to form a tight bundle phase, as the positively charged CS chains wrapped  
40 around DNA for charge matching caused a significant aggregation of DNA.  
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55 The DNA correlation peak associated with CS/DNA complexes was also observable in  
56 the SAXS profiles of NPs containing CS, DNA and  $\gamma$ -PGA. Interestingly, this peak was  
57 located at a higher  $q$  ( $3.0 \text{ nm}^{-1}$ ) than that associated with the binary CS/DNA complex,  
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4 showing that the incorporation of  $\gamma$ -PGA induced a more compact packing of DNA chains  
5 (with a reduction of  $d_{\text{DNA}}$  to 2.10 nm). Moreover, an excess intensity (marked by the arrow  
6 in Fig. 3a) was identified at lower  $q$  for the ternary system (CS/DNA/ $\gamma$ -PGA) and it became  
7 more significant at a higher content of  $\gamma$ -PGA. The presence of this intensity contribution  
8 implied the existence of a heterogeneity or domains with a characteristic length scale larger  
9 than  $d_{\text{DNA}}$  in NPs.  
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18 The features of SAXS patterns indicated that the NPs formed by the ternary system were  
19 composed of two types of domains containing CS/DNA and CS/ $\gamma$ -PGA complexes, as  
20 schematically illustrated in Fig. 3b. This type of NPs is called “compounded NPs” here. The  
21 dense packing of DNA chains in CS/DNA domains gave rise to the scattering peak, while  
22 the CS/ $\gamma$ -PGA domains surrounding the CS/DNA domains contributed to the excess  
23 intensity observed at lower  $q$ . In this case, the CS/ $\gamma$ -PGA domains might create a relatively  
24 rigid environment to suppress the positional distortion of the DNA chains induced by  
25 thermal fluctuations; as a result, the DNA chains in CS/DNA domains exhibited a more  
26 compact packing. In addition, we expected the presence of unbounded (or pendant) segments  
27 of CS chains emanating from the surface of CS/ $\gamma$ -PGA complexes; these pendant CS  
28 segments might subsequently bridge with the neighboring DNA chains to form two types of  
29 domains containing CS/ $\gamma$ -PGA and CS/DNA complexes within the compounded NPs (Fig.  
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5 *3.4. Percentage of cells transfected and gene expression level*  
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7 To determine the percentage of cells that actually expressed the transgene, we counted  
8 the number of EGFP-positive cells using flow cytometry at 48 h post transfection. As shown  
9 in Fig. 4a, only up to 15% of the cells produced EGFP when transfected with the NPs  
10 containing no  $\gamma$ -PGA (N/P/C ratio of 10/1/0, i.e., CS/DNA NPs). By incorporating  $\gamma$ -PGA in  
11 NPs (N/P/C ratios of 10/1/0.5 to 10/1/6), a significant increase in the percentage of cells that  
12 expressed EGFP was found. Transfection was increased approximately 4-fold (55%) for the  
13 cells transfected with the NPs with an N/P/C ratio of 10/1/4 compared to those treated with  
14 the NPs containing no  $\gamma$ -PGA ( $P < 0.05$ ).  
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22 The results of expression levels of EGFP or luciferase of cells are given in Fig. 4b and  
23 4c, respectively. As shown, the EGFP expression levels of cells transfected with the NPs  
24 incorporating  $\gamma$ -PGA were significantly higher than those treated with the NPs containing no  
25  $\gamma$ -PGA ( $P < 0.05$ ). The luciferase gene expression of cells transfected by the NPs with an  
26 N/P/C ratio of 10/1/4 was about 10-fold increased in comparison with those treated with the  
27 NPs containing no  $\gamma$ -PGA ( $P < 0.05$ ). These results indicated that the transfection efficiency  
28 of NPs was significantly enhanced after the incorporation of  $\gamma$ -PGA. Among all studied  
29 groups, the cells transfected with the NPs with an N/P/C ratio of 10/1/4 had the highest gene  
30 expression level.  
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40 *3.5. Cellular uptake*  
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42 CLSM was used to visualize the cellular uptake of Cy3-labeled NPs and their EGFP  
43 expression. The results of fluorescence images of cells after exposure to NPs prepared at  
44 different N/P/C ratios are shown in Fig. 5a and 5b. At 2 h after transfection, accumulation of  
45 Cy3-labeled NPs was observed in most of the incubated cells in all studied groups (Fig. 5a).  
46 The fluorescence intensity observed in cells increased notably with increasing the amount of  
47  $\gamma$ -PGA incorporated in NPs. At this time, no EGFP expression was observed for all of the  
48 studied groups. At 48 h after transfection, it appeared that the numbers of cells that  
49 expressed EGFP in the groups transfected with the NPs incorporating  $\gamma$ -PGA were more than  
50 the group treated with the NPs containing no  $\gamma$ -PGA (Fig. 5b).  
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5 After a 2-h transfection, the percentage of cells that internalized FITC-labeled NPs and  
6 their fluorescence intensity were quantified by flow cytometry. As shown in Fig. 5c and 5d,  
7 the percentage of fluorescent cells and their fluorescence intensity upon internalization of  
8 NPs were significantly enhanced with increasing the amount of  $\gamma$ -PGA incorporated ( $P <$   
9  $0.05$ ). However, there were no statistically significant differences between test NPs with  
10 N/P/C ratios of 10/1/4 and 10/1/6 ( $P > 0.05$ ).  
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16 To further elucidate differences in the uptake mechanism, the interaction of NPs with  
17 cell membranes was investigated by treating cells with trypsin at different concentrations  
18 prior to transfection. As shown in Fig. 6a, trypsinization resulted in a significant decrease in  
19 the internalization of FITC-labeled NPs with or without  $\gamma$ -PGA ( $P < 0.05$ ). However, trypsin  
20 did not induce a concentration-dependent effect on the uptake of the NPs containing no  
21  $\gamma$ -PGA (Fig. 6a and 6b,  $P > 0.05$ ), while it caused a concentration-dependent decrease in the  
22 internalization of the NPs incorporating  $\gamma$ -PGA (Fig. 6a and 6c,  $P < 0.05$ ). These results  
23 implied that by incorporating  $\gamma$ -PGA, test NPs might be internalized by cells via a specific  
24 protein-mediated endocytosis.  
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### 34 *3.6. MTT assay*

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36 Fig. 7 shows the viability of cells cultured in the media treated with varying test  
37 samples. As shown, the cytotoxicity of naked DNA,  $\gamma$ -PGA and CS was quite low. The  
38 viability of the cells treated with test NPs decreased relatively with increasing the amount of  
39  $\gamma$ -PGA incorporated.  
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## 46 **4. Discussion**

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48 CS/DNA complex NPs have been considered as a candidate for gene delivery [23–24].  
49 Although advantageous for DNA packing and protection, CS-based complexes may lead to  
50 difficulties in DNA release once they arrive at the site of action [11], thus limiting their  
51 transfection efficiency. In the study, we demonstrated that after the incorporation of  $\gamma$ -PGA  
52 in CS/DNA NPs, the percentage of cells transfected and their gene expression level were  
53 significantly enhanced (Fig. 4a–4c and 5b).  
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5 The pKa values of CS and  $\gamma$ -PGA are 6.5 and 2.9, respectively [25]. When prepared in  
6 DI water (pH 6.0), CS, DNA and  $\gamma$ -PGA are ionized. The ionized CS, DNA and  $\gamma$ -PGA can  
7 form polyelectrolyte complexes (CS/DNA/ $\gamma$ -PGA NPs) by electrostatic interactions between  
8 the positively charged amino groups ( $-\text{NH}_3^+$ ) on CS and the negatively charged phosphate  
9 groups ( $-\text{PO}_4^-$ ) on DNA and carboxyl groups ( $-\text{COO}^-$ ) on  $\gamma$ -PGA.

10  
11 The SAXS results revealed that DNA and  $\gamma$ -PGA formed complexes with CS separately  
12 to yield two types of domains bridged by pendant CS chains in the compounded NPs (Fig.  
13 3b) [9,26]. After internalization into cells, the compounded NPs would be expected to  
14 disintegrate into a number of even smaller sub-particles composing CS/DNA and CS/ $\gamma$ -PGA  
15 complexes, due to deprotonation of the bridged CS chains. The subsequent release of DNA  
16 through the disruption of these sub-particles became relatively easier than that from the  
17 larger CS/DNA NPs prepared without adding  $\gamma$ -PGA, because of their significantly greater  
18 specific surface area. Therefore, the compounded NPs prepared by incorporating  $\gamma$ -PGA not  
19 only offered a protection of loaded DNA in the course of delivery but also enhanced the  
20 release of DNA within cells [24].

21  
22 However, as the amount of  $\gamma$ -PGA incorporated was increased to a critical value, the  
23 transfection efficiency of CS/DNA/ $\gamma$ -PGA NPs (N/P/C ratio of 10/1/6) started to drop  
24 appreciably (Fig. 4a and 4b). When beyond this threshold, there might be too many  
25 dissociated DNA molecules exposed to cytosolic nuclease(s), thus leading to their  
26 degradation before entry of the nucleus [27]. As indicated in Fig. 3c, with increasing the  
27 amount of  $\gamma$ -PGA incorporated in CS/DNA/ $\gamma$ -PGA NPs, DNA was more susceptible to  
28 enzymatic degradation in the environments simulating the cytoplasm and nuclei.

29  
30 Interestingly, in addition to improving the release of DNA intracellularly, the  
31 incorporation of  $\gamma$ -PGA in test NPs significantly enhanced their cellular internalization (Fig.  
32 5a, 5c and 5d). Cellular entry can be realized by distinct mechanisms that may lead to  
33 disparate percentages of cellular uptake and therefore different transfection efficiencies [28].  
34 It is known that a number of polyplexes can induce cellular internalization through a  
35 non-specific charge-mediated interaction with proteoglycans that are present on cell  
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5 membranes [29]. These highly anionic proteoglycans determine much of the interactions  
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7 between the cell surface and extracellular macromolecules [30] and believed to play an  
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9 important role in the cellular uptake of many non-targeted, positively charged gene delivery  
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11 vectors [29,31].

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13 Trypsinization resulted in a substantial reduction in surface-bound proteins on the cell  
14  
15 surface. As shown in Fig. 6a and 6b, after trypsinization, a remarkable decrease in the  
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17 percentage of cellular uptake of CS/DNA NPs was observed; however, this phenomenon was  
18  
19 in a trypsin concentration-independent manner. These results implied that the internalization  
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21 of CS/DNA NPs might be mainly via a non-specific charge-mediated interaction between the  
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23 NPs (positively charged) and the components of cell membranes (negatively charged  
24  
25 proteoglycans, Fig. 8a) [11].

26  
27 In contrast, a trypsin concentration-dependent reduction of the cellular uptake of  
28  
29 CS/DNA/ $\gamma$ -PGA NPs was observed (Fig. 6a and 6c). This observation suggested that besides  
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31 a non-specific charged-mediated binding to cell membranes, there were specific  
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33 trypsin-cleavable proteins involved in the internalization of CS/DNA/ $\gamma$ -PGA NPs (Fig. 8b),  
34  
35 indicating that  $\gamma$ -PGA played a crucial role in the cellular uptake of CS/DNA/ $\gamma$ -PGA NPs.  
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37 This might explain why there was a significantly more cellular internalization of  
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39 CS/DNA/ $\gamma$ -PGA NPs than their CS/DNA counterparts (Fig. 5a, 5c and 5d). However, the  
40  
41 exact mechanism by which these specific membrane-present proteins mediate the cellular  
42  
43 uptake of CS/DNA/ $\gamma$ -PGA NPs remains to be understood.

## 44 45 46 **5. Conclusions**

47  
48 A new CS-based NP system incorporating  $\gamma$ -PGA was developed in the study as an  
49  
50 efficient vector for gene delivery. The analysis of our SAXS results indicated that  
51  
52 incorporating  $\gamma$ -PGA would cause the formation of compounded NPs whose internal  
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54 structure might facilitate the dissociation of CS and DNA. In addition to improving the  
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56 release of DNA intracellularly, the incorporation of  $\gamma$ -PGA in NPs markedly increased their  
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58 cellular internalization. Taken together,  $\gamma$ -PGA significantly enhanced the transfection  
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5 efficiency of this newly developed gene-delivery system.  
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9 **Acknowledgments**

10 This work was supported by a grant from the National Science Council  
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12 experiment supported by the NSRRC under Project ID 2007-1-018-4 was gratefully  
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5 **References**

- 6 [1] Jin J, Song M, Hourston DJ. Novel chitosan-based films cross-linked by genipin with  
7 improved physical properties. *Biomacromolecules* 2004;5:162-8.  
8  
9 [2] Iwasaki N, Yamane ST, Majima T, Kasahara Y, Minami A, Harada K, et al. Feasibility of  
10 polysaccharide hybrid materials for scaffolds in cartilage tissue engineering: evaluation  
11 of chondrocyte adhesion to polyionic complex fibers prepared from alginate and  
12 chitosan. *Biomacromolecules* 2004;5:828-33.  
13  
14 [3] Mao HQ, Roy K, Troung-Le VL, Janes KA, Lin KY, Wang Y, et al. Chitosan-DNA  
15 nanoparticles as gene carriers: synthesis, characterization and transfection efficiency. *J*  
16 *Controlled Release* 2001;70:399-421.  
17  
18 [4] Kim TH, Park IK, Nah JW, Choi YJ, Cho CS. Galactosylated chitosan/DNA  
19 nanoparticles prepared using water-soluble chitosan as a gene carrier. *Biomaterials*  
20 2004;25: 3783-92.  
21  
22 [5] Morille M, Passirani C, Vonarbourg A, Clavreul A, Benoit JP. Progress in developing  
23 cationic vectors for non-viral systemic gene therapy against cancer. *Biomaterials* 2008;  
24 29:3477-96.  
25  
26 [6] Kim TH, Jiang HL, Jere D, Park IK, Cho MH, Nah JW, et al. Chemical modification of  
27 chitosan as a gene carrier in vitro and in vivo. *Prog Polym Sci* 2007;32:726-53.  
28  
29 [7] Lee MK, Chun SK, Choi WJ, Kim JK, Choi SH, Kim A, et al. The use of chitosan as a  
30 condensing agent to enhance emulsion-mediated gene transfer. *Biomaterials* 2005;  
31 26:2147-56.  
32  
33 [8] Lavertu M, Méthot S, Tran-Khanh N, Buschmann MD. High efficiency gene transfer  
34 using chitosan/DNA nanoparticles with specific combinations of molecular weight and  
35 degree of deacetylation. *Biomaterials* 2006;27:4815-24.  
36  
37 [9] Lee PW, Peng SF, Su CJ, Mi FL, Chen HL, Wei MC, et al. The use of biodegradable  
38 polymeric nanoparticles in combination with a low-pressure gene gun for transdermal  
39 DNA delivery. *Biomaterials* 2008;29:742-51.  
40  
41 [10] Douglas KL, Piccirillo CA, Tabrizian M. Effects of alginate inclusion on the vector  
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46  
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5 properties of chitosan-based nanoparticles. *J Controlled Release* 2006;115:354-61.  
6  
7 [11] Wong SY, Pelet J, Putnam D. Polymer systems for gene delivery—Past, present, and  
8 future. *Prog Polym Sci* 2007;32:799-837.  
9  
10 [12] Lin YH, Mi FL, Chen CT, Chang WC, Peng SF, Liang HF, et al. Preparation and  
11 characterization of nanoparticles shelled with chitosan for oral insulin delivery.  
12 *Biomacromolecules* 2007;8:146-52.  
13  
14 [13] Mi FL, Wu YY, Lin YH, Sonaje K, Ho YC, Chen CT, et al. Oral delivery of peptide  
15 drugs using nanoparticles self-assembled by poly( $\gamma$ -glutamic acid) and a chitosan  
16 derivative functionalized by trimethylation. *Bioconjug Chem* 2008;19:1248-55.  
17  
18 [14] Wang X, Uto T, Akagi T, Akashi M, Baba M. Poly( $\gamma$ -glutamic acid) nanoparticles  
19 as an efficient antigen delivery and adjuvant system: potential for an AIDS vaccine. *J*  
20 *Med Virol* 2008;80:11-9.  
21  
22 [15] Cui Z, Mumper RJ. Chitosan-based nanoparticles for topical genetic immunization. *J*  
23 *Controlled Release* 2001;75:409-19.  
24  
25 [16] Adams CWM. Osmium tetroxide and the marchi method: reactions with polar and  
26 non-polar lipids, protein and polysaccharide. *J Histochem Cytochem* 1960;8:262-7.  
27  
28 [17] Hsu WL, Li YC, Chen HL, Liou W, Jeng US, Lin HK, et al. Thermally-induced  
29 order-order transition of DNA-cationic surfactant complexes. *Langmuir*  
30 2006;22:7521-7.  
31  
32 [18] Ko IK, Ziady A, Lu S, Kwon YJ. Acid-degradable cationic methacrylamide  
33 polymerized in the presence of plasmid DNA as tunable non-viral gene carrier.  
34 *Biomaterials* 2008;29:3872-81.  
35  
36 [19] Qaqish RB, Amiji MM. Synthesis of a fluorescent chitosan derivative and its  
37 application for the study of chitosan-mucin interactions. *Carbohydr Polym*  
38 1999;38:99-107.  
39  
40 [20] Ho YP, Chen HH, Leong KW, Wang TH. Evaluating the intracellular stability and  
41 unpacking of DNA nanocomplexes by quantum dots-FRET. *J Controlled Release*  
42 2006;116:83-9.  
43  
44  
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46  
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4  
5 [21] Szolnoky G, Bata-Csörgö Z, Kenderessy AS, Kiss M, Pivarcsi A, Novák Z, et al. A  
6 mannose-binding receptor is expressed on human keratinocytes and mediates killing of  
7 *Candida albicans*. J Invest Dermatol 2001;117:205-13.  
8  
9  
10 [22] Liang HF, Yang TF, Huang CT, Chen MC, Sung HW. Preparation of nanoparticles  
11 composed of poly(gamma-glutamic acid)-poly(lactide) block copolymers and  
12 evaluation of their uptake by HepG2 cells. J Controlled Release 2005;105:213-25.  
13  
14 [23] Dang JM, Leong KW. Natural polymers for gene delivery and tissue engineering. Adv  
15 Drug Deliv Rev 2006;58:487-99.  
16  
17 [24] Kiang T, Wen J, Lim HW, Leong KW. The effect of the degree of chitosan  
18 deacetylation on the efficiency of gene transfection. Biomaterials 2004;25:5293-301.  
19  
20 [25] Lin YH, Chen CT, Liang HF, Kulkarni AR, Lee PW, Chen CH, et al. Novel  
21 nanoparticles for oral insulin delivery via the paracellular pathway. Nanotechnology  
22 2007;18:105102.  
23  
24 [26] DeRouchey J, Netz RR, Rädler JO. Structural investigations of DNA-polycation  
25 complexes. Eur Phys J E Soft Matter 2005;16:17-28.  
26  
27 [27] Lechardeur D, Sohn KJ, Haardt M, Joshi PB, Monck M, Graham RW, et al. Metabolic  
28 instability of plasmid DNA in the cytosol: a potential barrier to gene transfer. Gene  
29 Ther 1999;6:482-97.  
30  
31 [28] Douglas KL, Piccirillo CA, Tabrizian M. Cell line-dependent internalization pathways  
32 and intracellular trafficking determine transfection efficiency of nanoparticle vectors.  
33 Eur J Pharm Biopharm 2008;68:676-87.  
34  
35 [29] Mislick KA, Baldeschwieler JD. 1996. Evidence for the role of proteoglycans in  
36 cation-mediated gene transfer. Proc Natl Acad Sci U S A 1996;93:12349-54.  
37  
38 [30] Yanagishita M, Hascall VC. Cell surface heparan sulfate proteoglycans. J Biol Chem  
39 1992;267:9451-4.  
40  
41 [31] Kichler A, Mason AJ, Bechinger B. Cationic amphipathic histidine-rich peptides for  
42 gene delivery. Biochim Biophys Acta 2006;1758:301-7.  
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**Figure Captions**

Figure 1. (a) Gel retardation analyses of CS/DNA complex nanoparticles prepared at different N/P ratios. Samples were run on a 0.8% agarose gel and subsequently stained using ethidium bromide. Complete complexation of DNA was noted at an N/P ratio of 10/1; (b) Gel retardation analyses of CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios.

Figure 2. TEM micrographs of CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios.

Figure 3. (a) SAXS profiles of CS/ $\gamma$ -PGA, CS/DNA and CS/DNA/ $\gamma$ -PGA complex nanoparticles. The arrow marks the excess intensity arising from the CS/ $\gamma$ -PGA domains in complexes formed in the ternary system (CS/DNA/ $\gamma$ -PGA nanoparticles); (b) Schematic illustrations of the internal structures of CS/DNA and CS/DNA/ $\gamma$ -PGA complex nanoparticles; (c) Agarose gel electrophoresis of the DNA released from CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios. Prior to electrophoresis, test nanoparticles were exposed in a phosphate buffered saline at pH 7.2 and then treated with restriction enzymes [*Bam*HI (B) and *Hind*III (H)], simulating the pH environments in the cytoplasm and nuclei.

Figure 4. Efficiencies of cell transfection: (a) percentages of cells that were transfected; (b) relative fluorescence intensities of transfected cells that expressed EGFP protein; (c) normalized luciferase activities of transfected cells that expressed the luciferase. Cells were transfected *in vitro* using CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios (n = 5). NC: negative control (the group without any treatment); NK: naked DNA; LF: Lipofectamine™ 2000.

Figure 5. (a) Confocal images of cells transfected with Cy3-labeled CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios for 2 h; (b) EGFP expressions of cells transfected with Cy3-labeled CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios for 48 h; (c) Percentages of cellular uptake of FITC-labeled CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios, analyzed by flow

cytometry (n = 3); (d) Intracellular fluorescence intensities of CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios determined by flow cytometry. NC: negative control (the group without any treatment).

Figure 6. Results of intracellular uptake of CS/DNA and CS/DNA/ $\gamma$ -PGA (N/P/C ratio of 10/1/4) nanoparticles after the cells being treated with different concentrations of trypsin, determined by flow cytometry: (a) percentages of intracellular uptake of test nanoparticles (n = 3); (b) fluorescence intensities after intracellular uptake of CS/DNA nanoparticles; (c) fluorescence intensities after intracellular uptake of CS/DNA/ $\gamma$ -PGA nanoparticles.

Figure 7. Results of the cell viability after being treated with CS/DNA/ $\gamma$ -PGA nanoparticles prepared at different N/P/C ratios determined by the MTT assay (n = 5). NC: negative control (the group without any treatment); NK: naked DNA;  $\gamma$ -PGA: poly( $\gamma$ -glutamic acid); CS: chitosan; LF: Lipofectamine<sup>TM</sup> 2000.

Figure 8. Schematic illustrations of potential uptake pathways: (a) CS/DNA nanoparticles. The internalization of CS/DNA nanoparticles might be mainly via a non-specific charge-mediated interaction between the nanoparticles (positively charged) and the components of cell membranes (negatively charged proteoglycans); (b) CS/DNA/ $\gamma$ -PGA nanoparticles. Besides a non-specific charged-mediated binding to cell membranes, there were specific trypsin-cleavable proteins involved in the internalization of CS/DNA/ $\gamma$ -PGA nanoparticles.

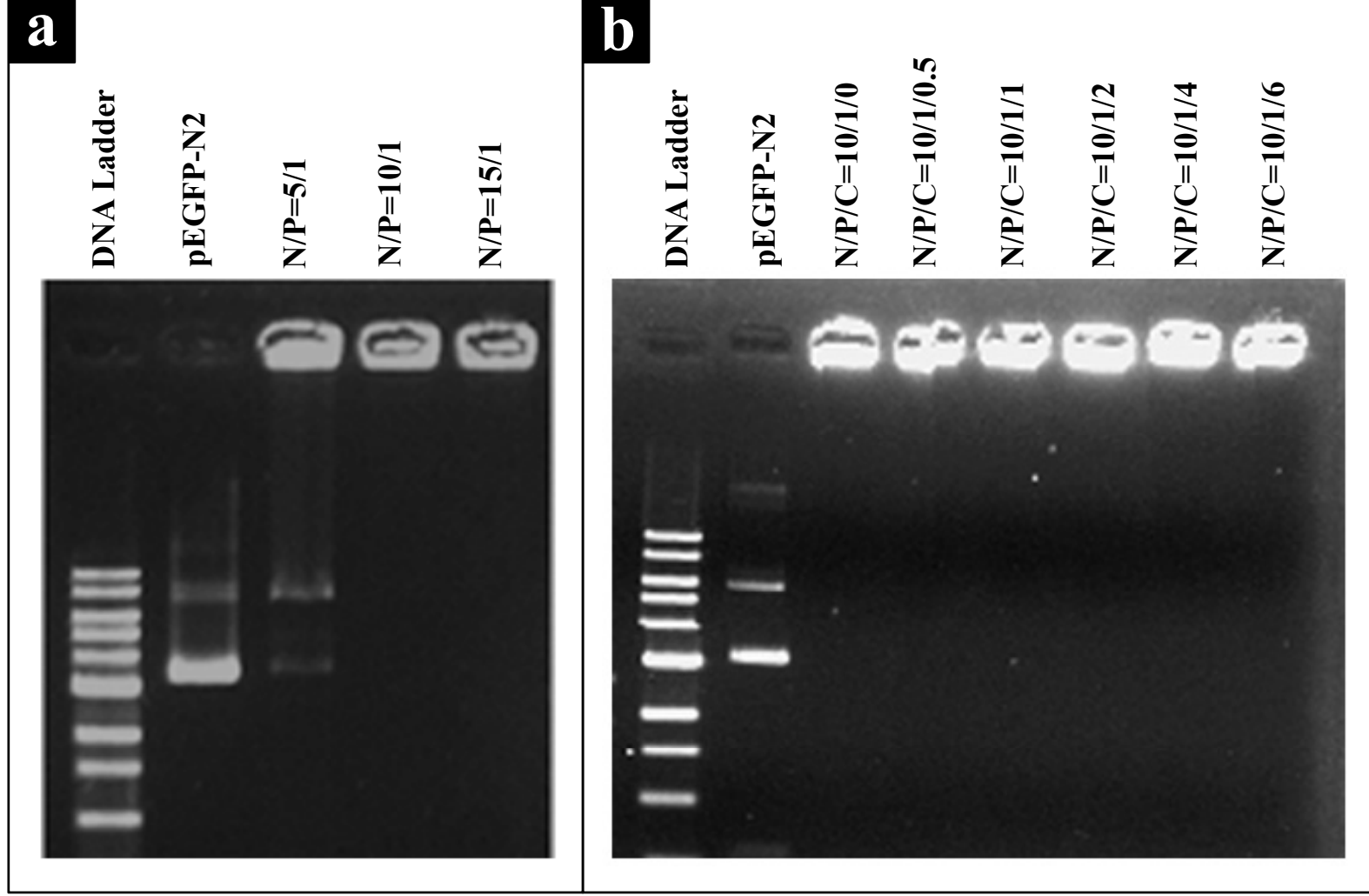


**Table**

Table 1. Size, polydispersity index (PI), zeta potential and encapsulation efficiency (EE) of pEGFP-N2 of test nanoparticles prepared at distinct N/P/C ratios (n = 5).

<b>N/P/C Ratio</b>	<b>Size (nm)</b>	<b>PI</b>	<b>Zeta Potential (mV)</b>	<b>EE (%)</b>
<b>N/P/C=10/1/0</b>	140.2±7.7	0.33±0.04	31.7±0.8	97.7±0.4
<b>N/P/C=10/1/0.5</b>	135.5±3.2	0.21±0.01	35.3±0.3	97.3±0.9
<b>N/P/C=10/1/1</b>	130.8±1.3	0.20±0.01	34.5±0.2	96.1±0.6
<b>N/P/C=10/1/2</b>	132.8±4.9	0.22±0.03	33.3±1.1	94.2±0.4
<b>N/P/C=10/1/4</b>	152.5±5.1	0.16±0.02	28.7±1.2	99.5±0.1
<b>N/P/C=10/1/6</b>	204.5±3.7	0.11±0.01	18.7±0.2	99.5±0.1

Figure 1



**Figure 2**

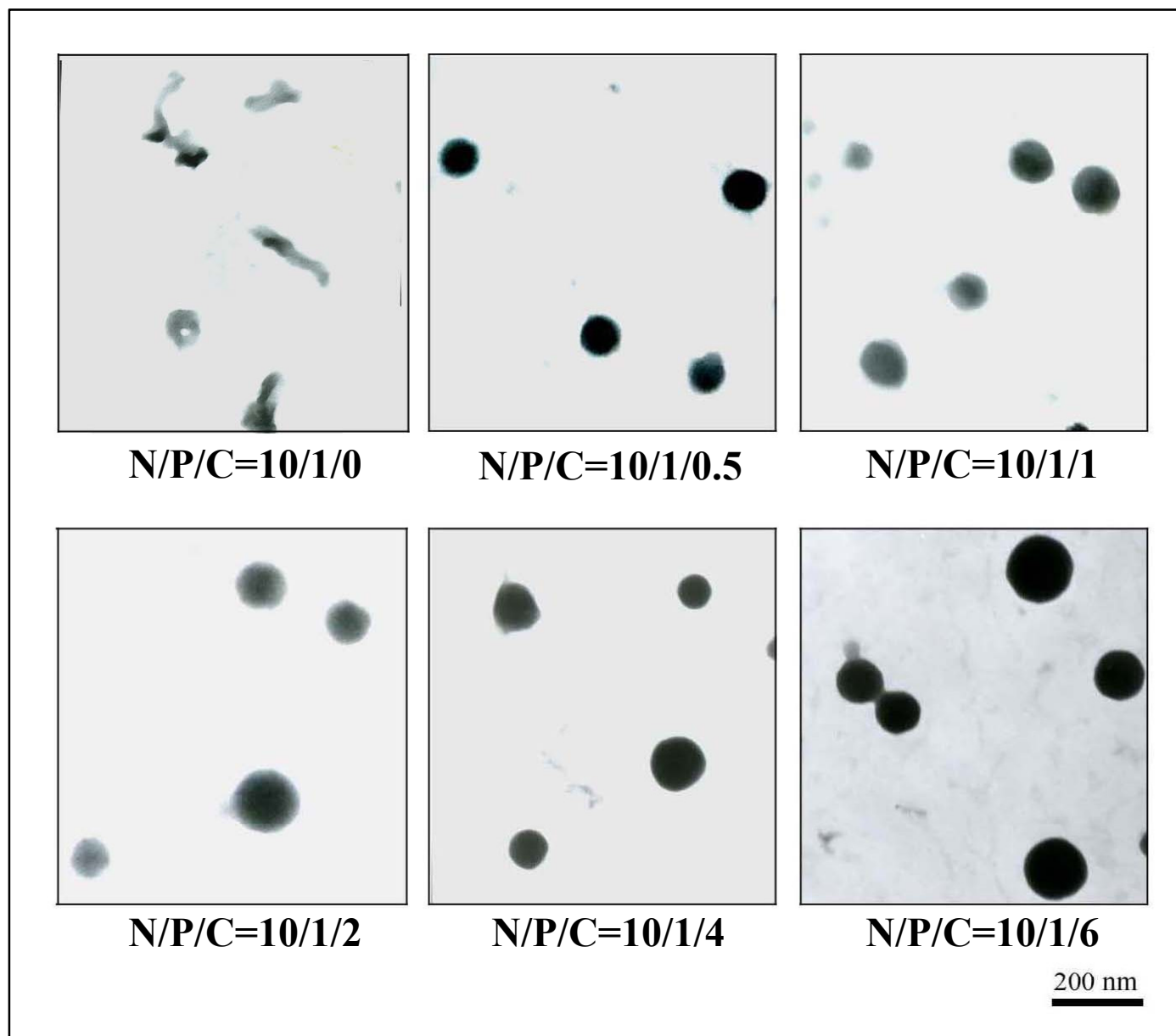


Figure 3

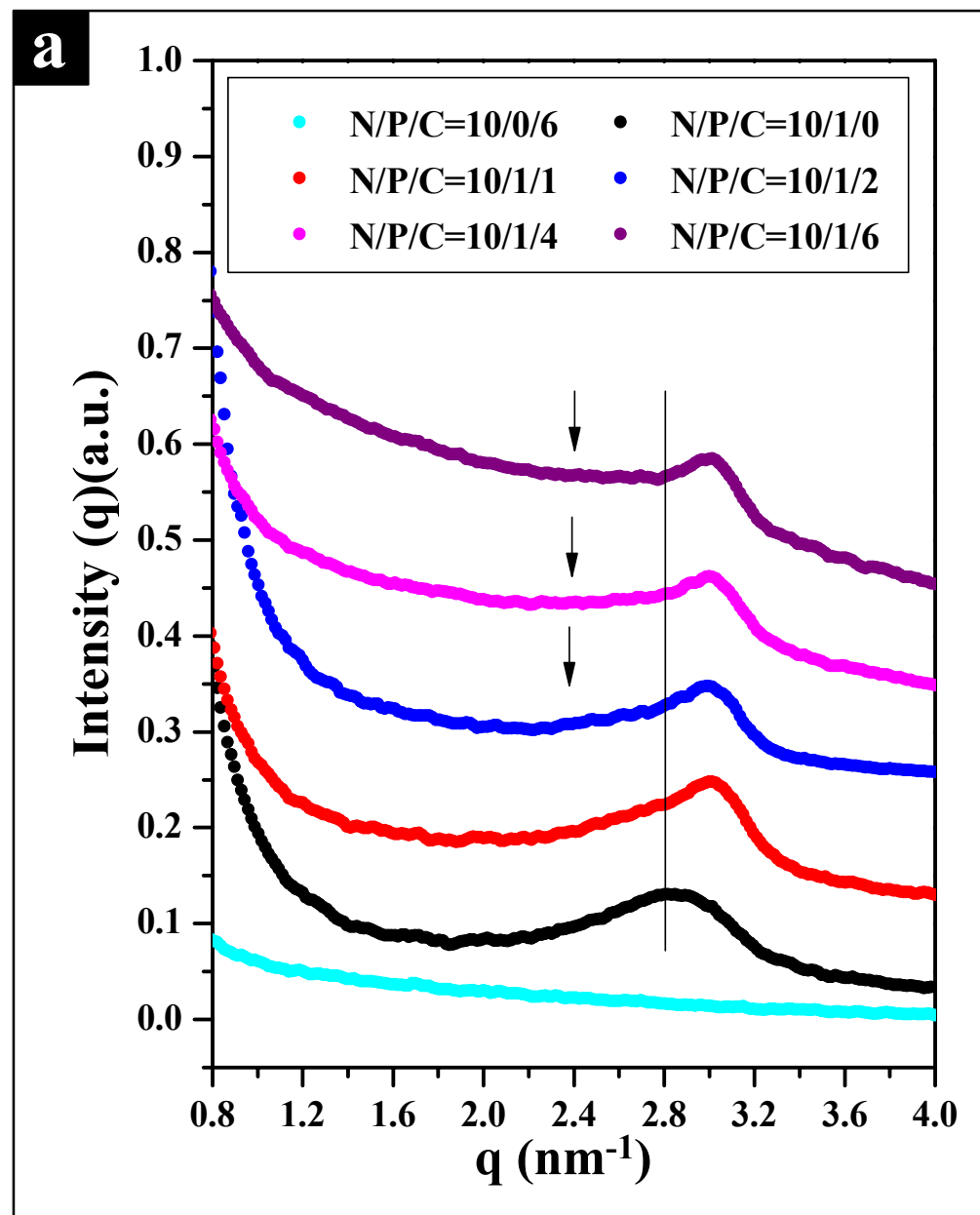
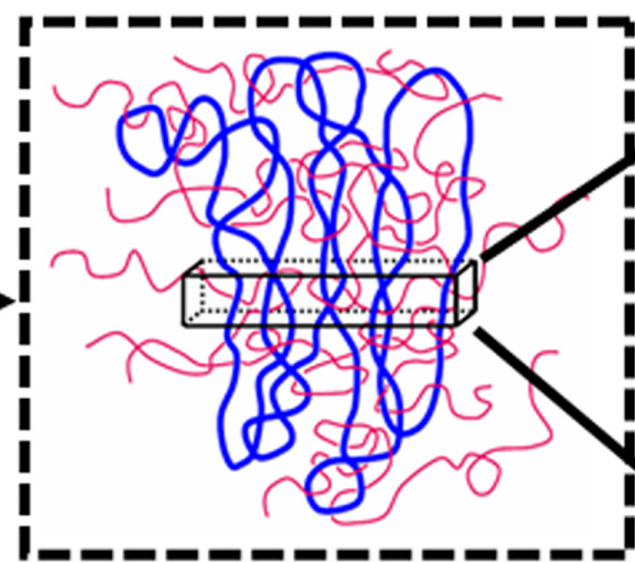
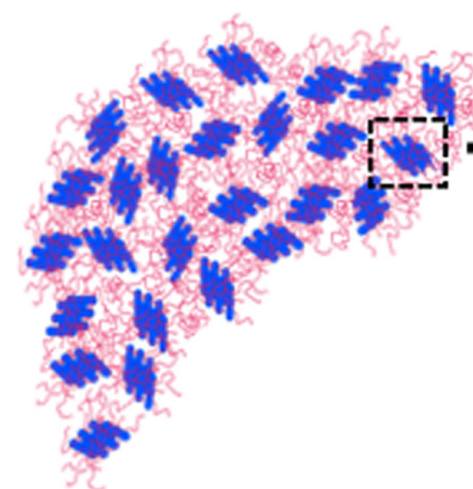


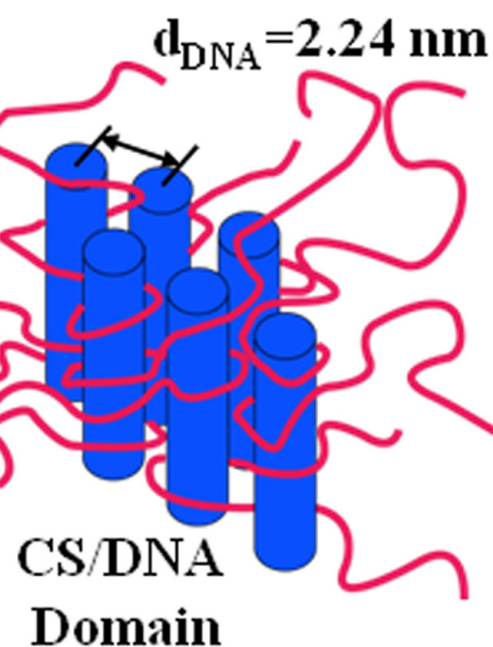
Figure 3b

**b**

**CS/DNA Complexes**

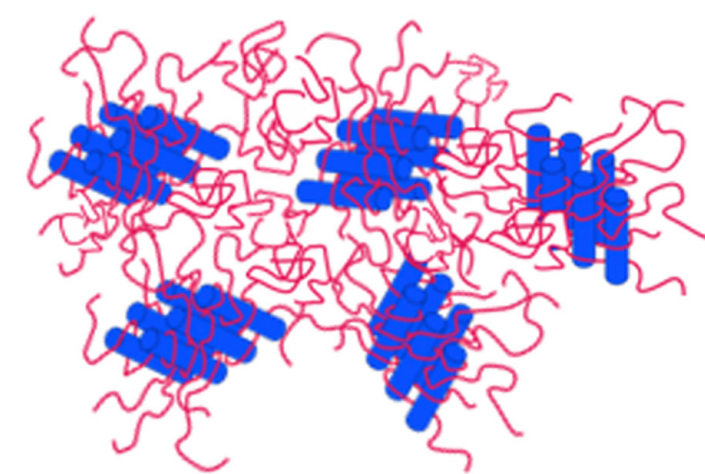


CS/DNA  
Domain



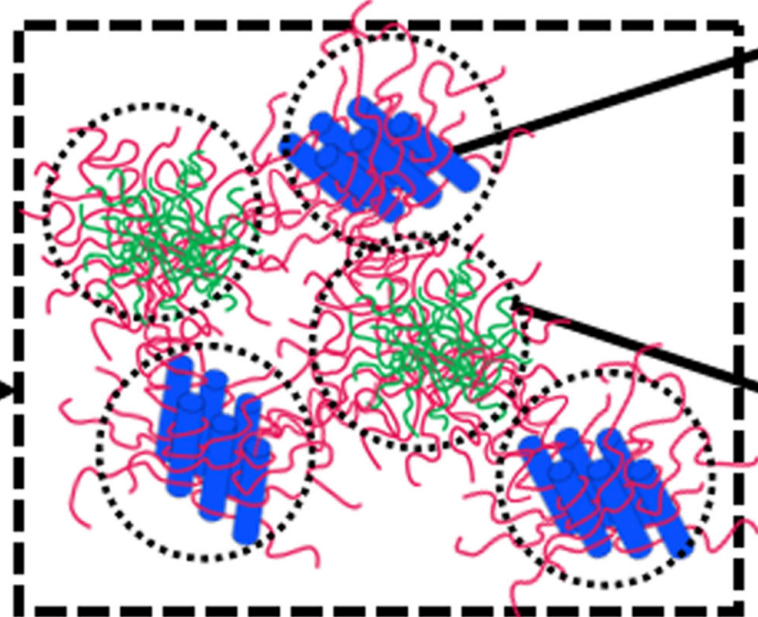
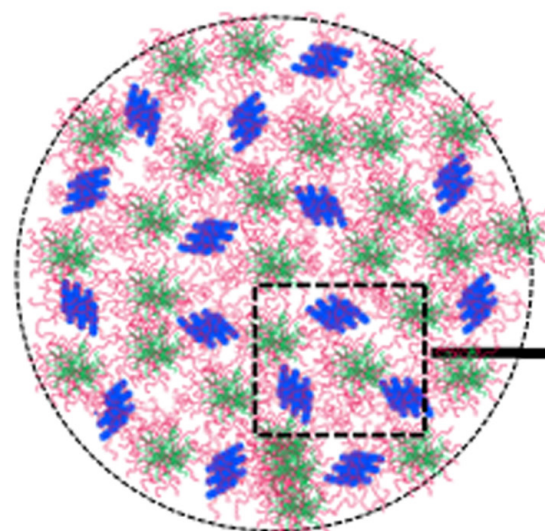
CS/DNA  
Domain

Shortly after  
Endocytosis

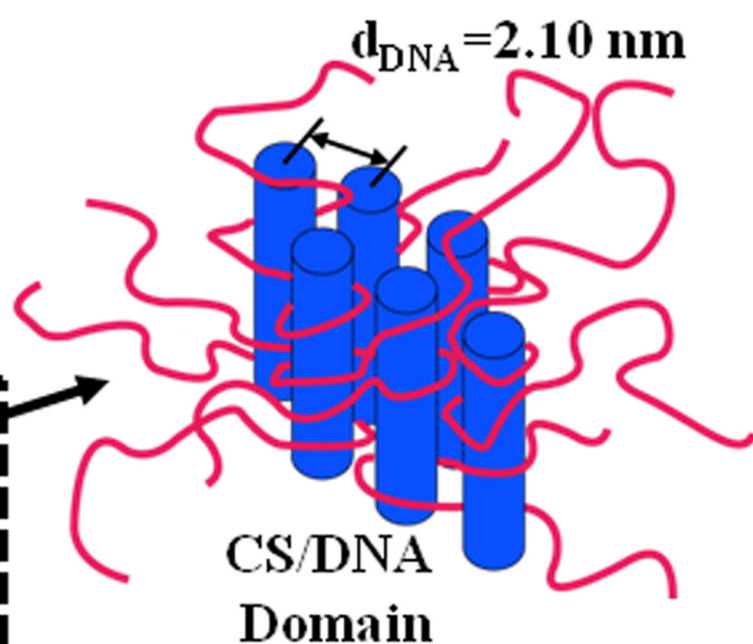


Deprotonation of  
CS Chains

**CS/DNA/  $\gamma$ -PGA Complexes  
(Compounded NPs)**

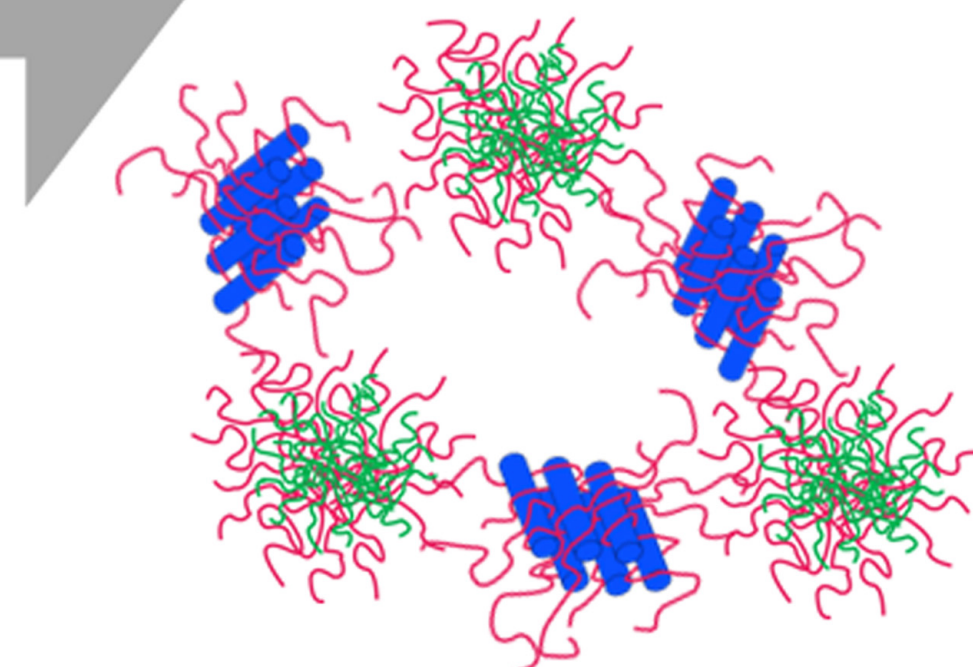


CS/DNA and CS/  $\gamma$ -PGA Domains  
Bridged by Pendant CS Chains

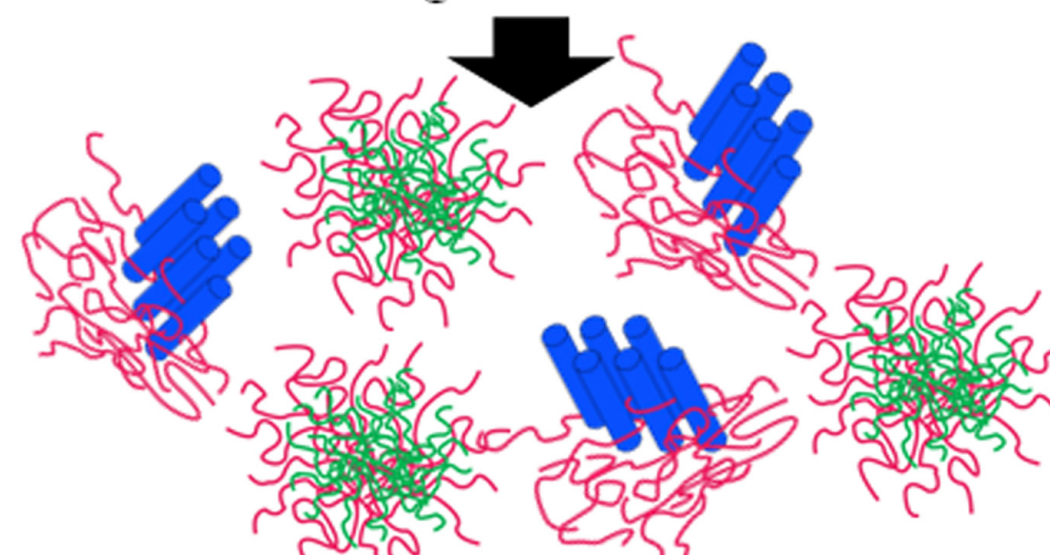


CS/DNA  
Domain

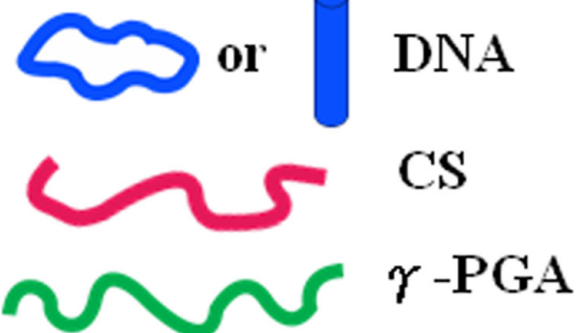
CS/  $\gamma$ -PGA  
Domain



Deprotonation of  
Bridged CS Chains



Dissociation of CS/DNA and  
CS/  $\gamma$ -PGA Domains

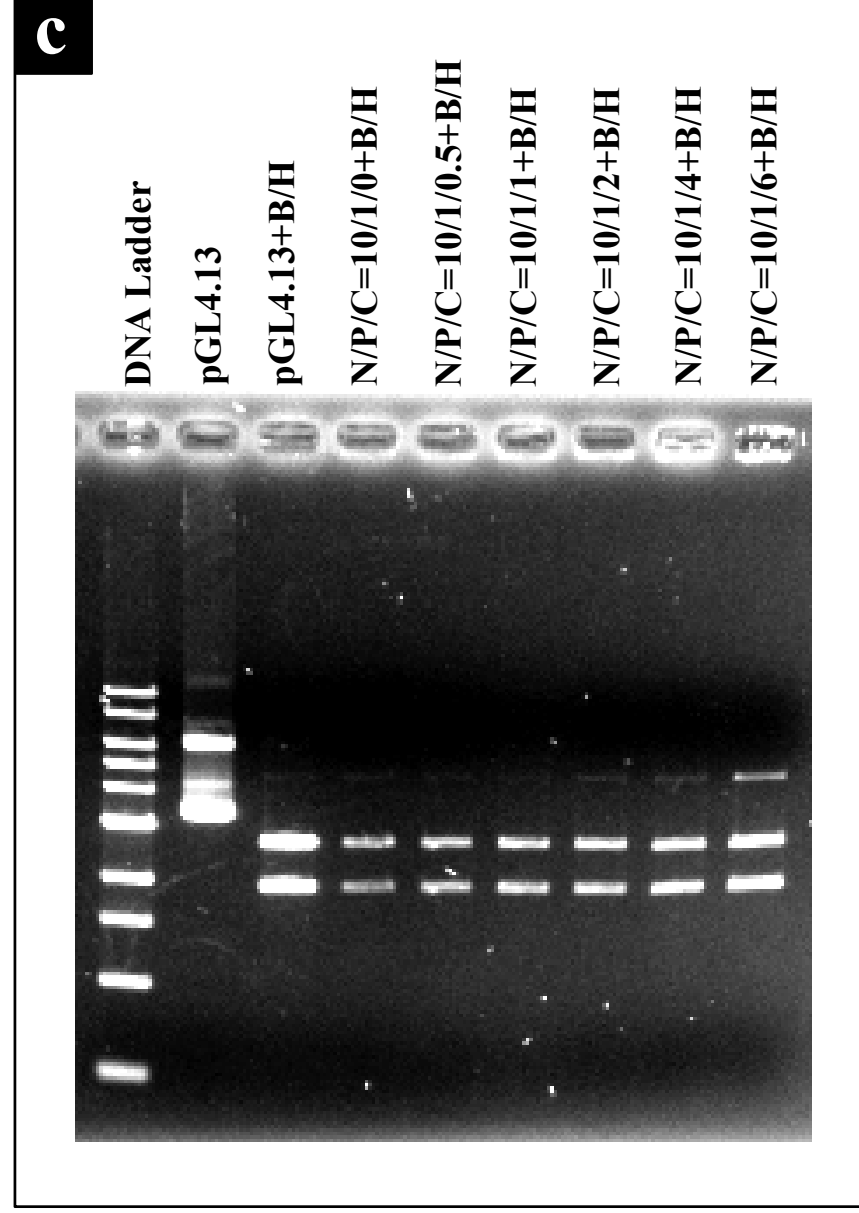


DNA

CS

$\gamma$ -PGA

Figure 3



**Figure 4**

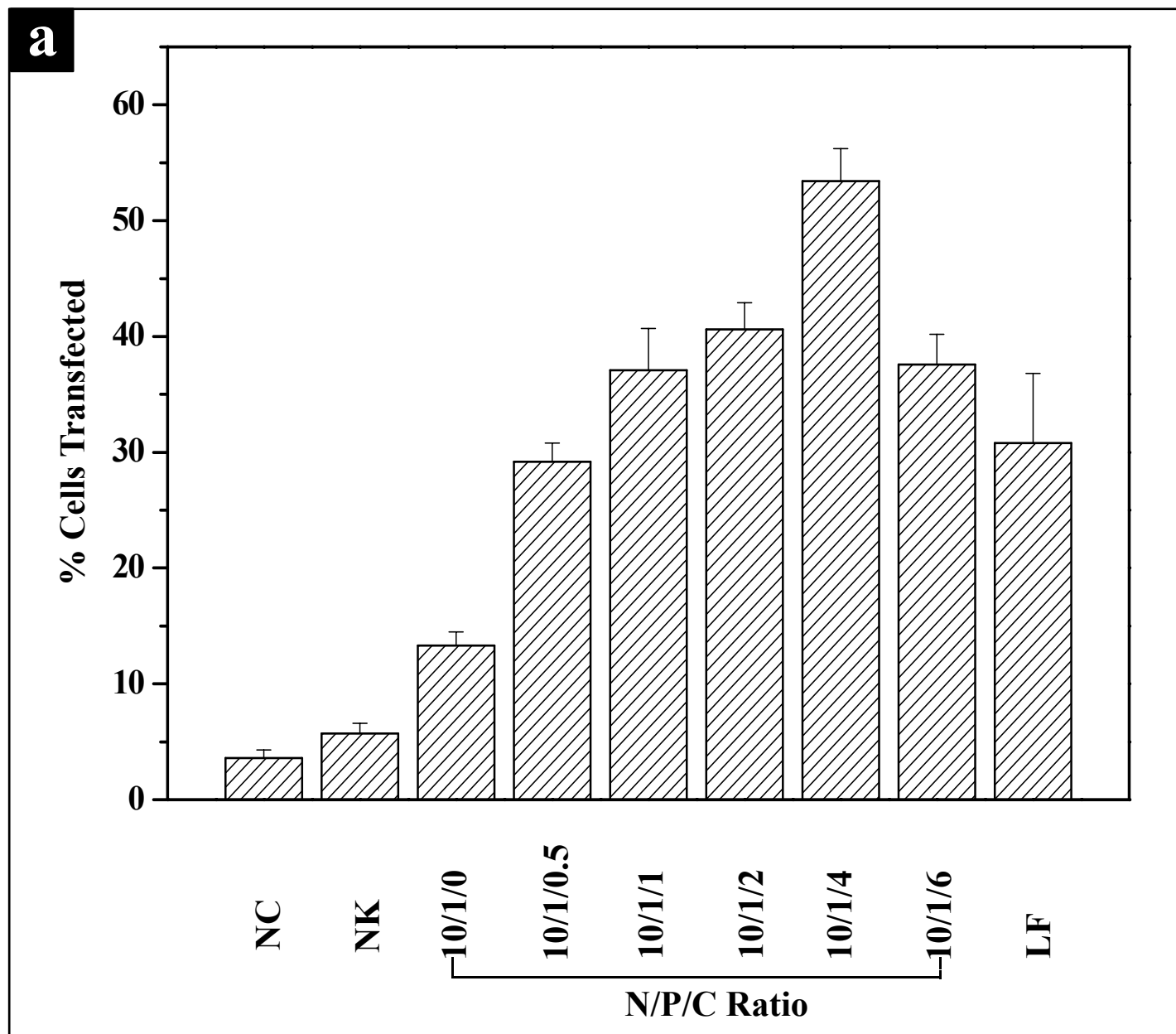


Figure 4

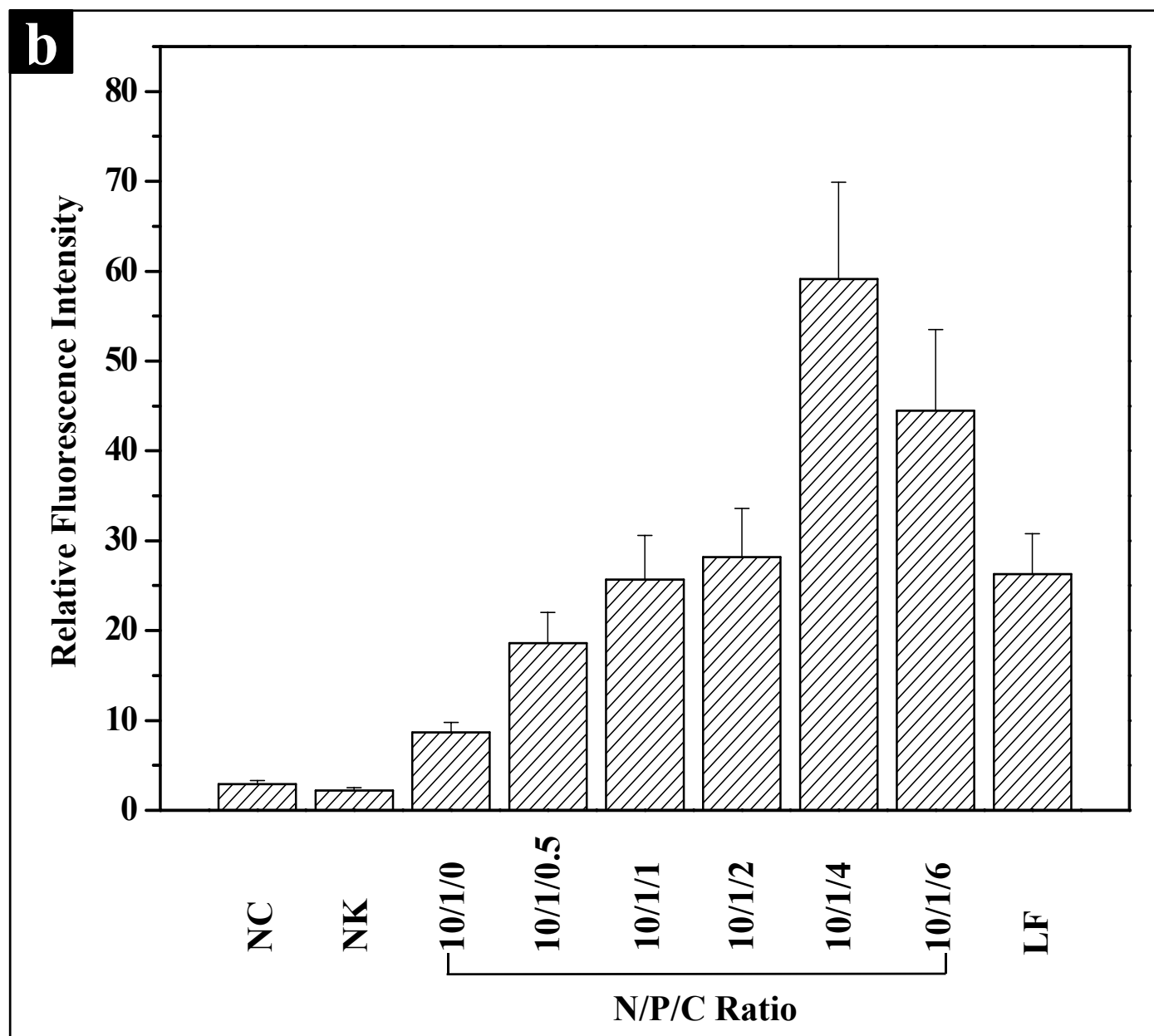




Figure 4

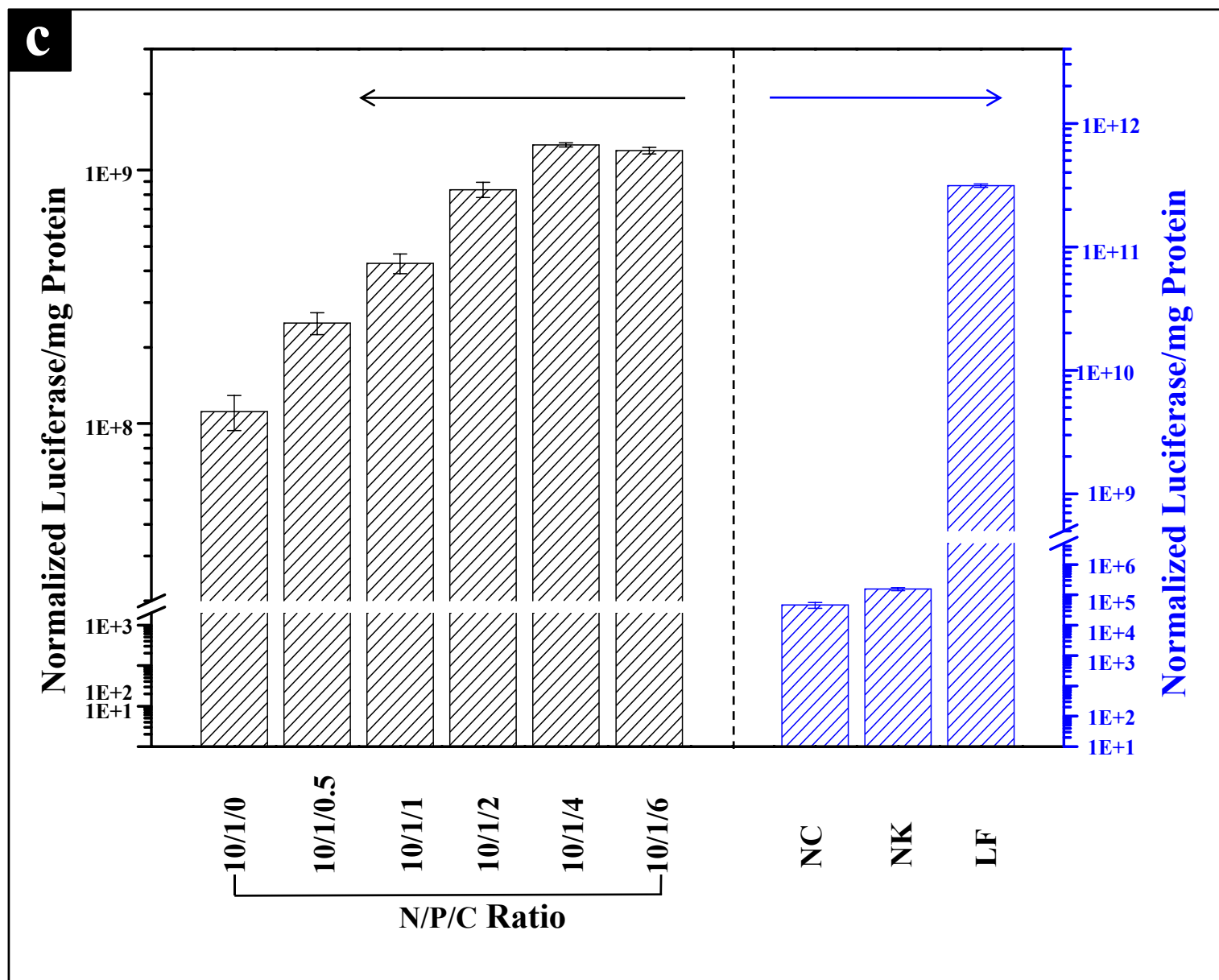
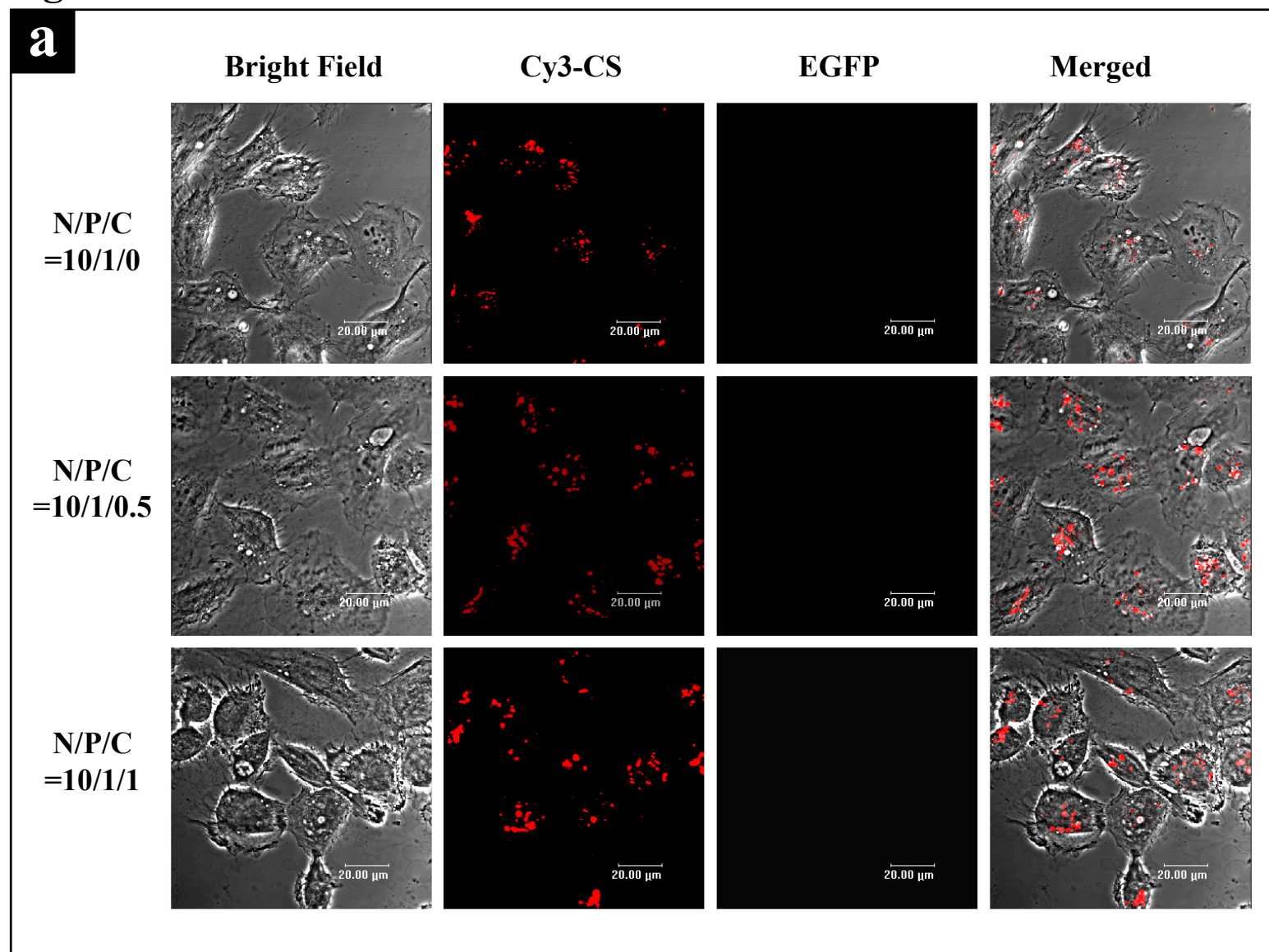


Figure 5



# Figure 5 Continued

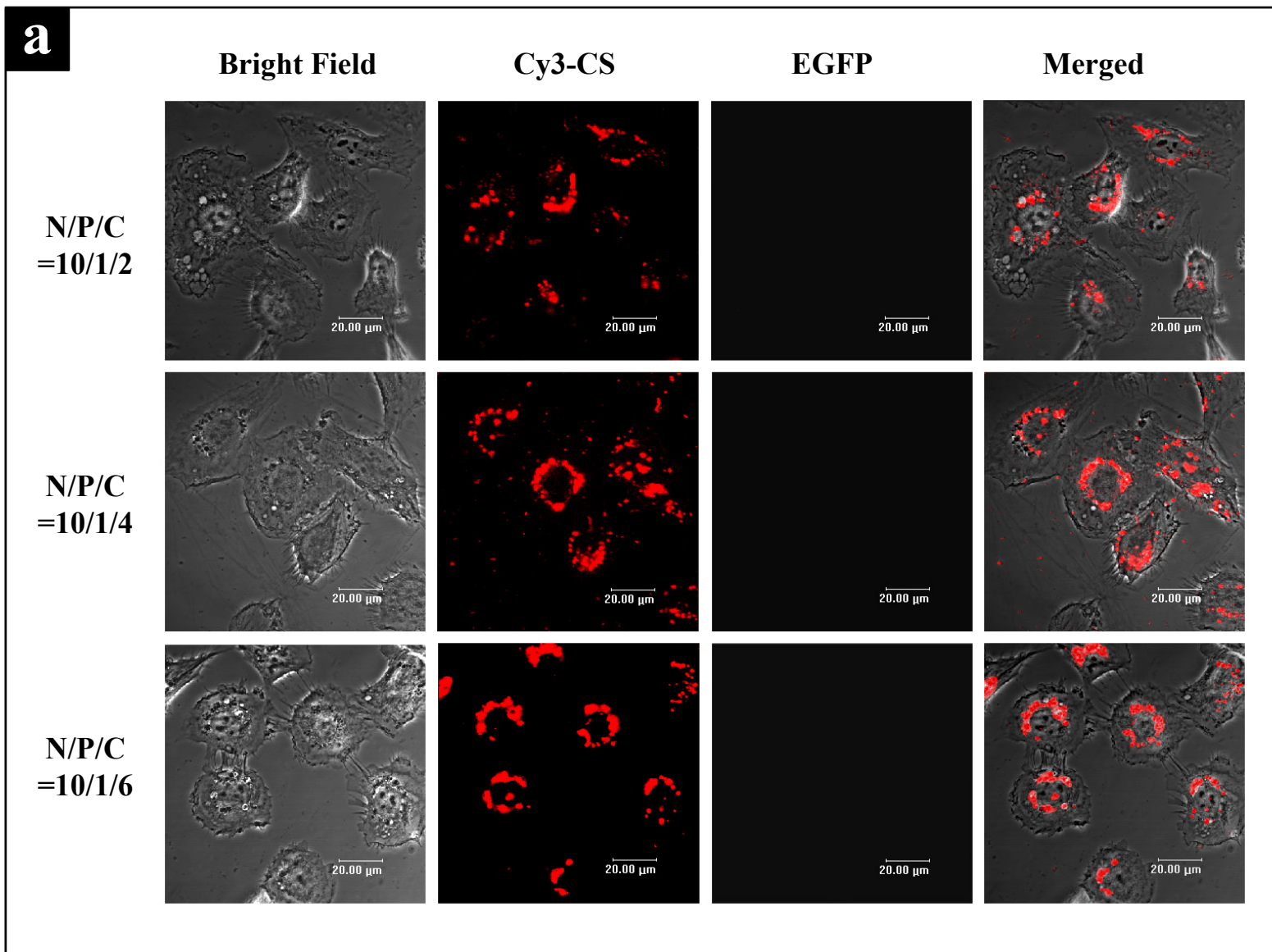


Figure 5

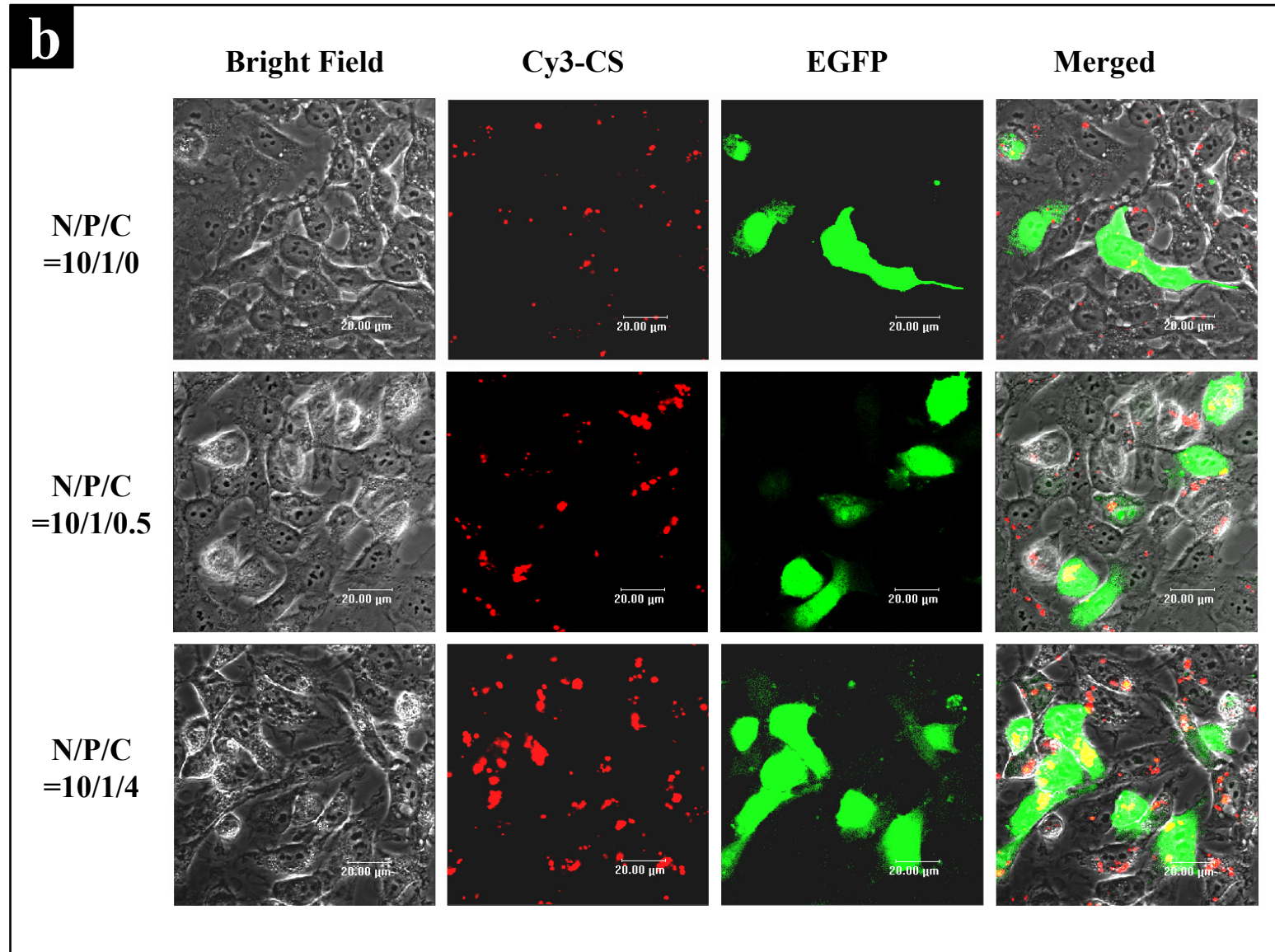


Figure 5

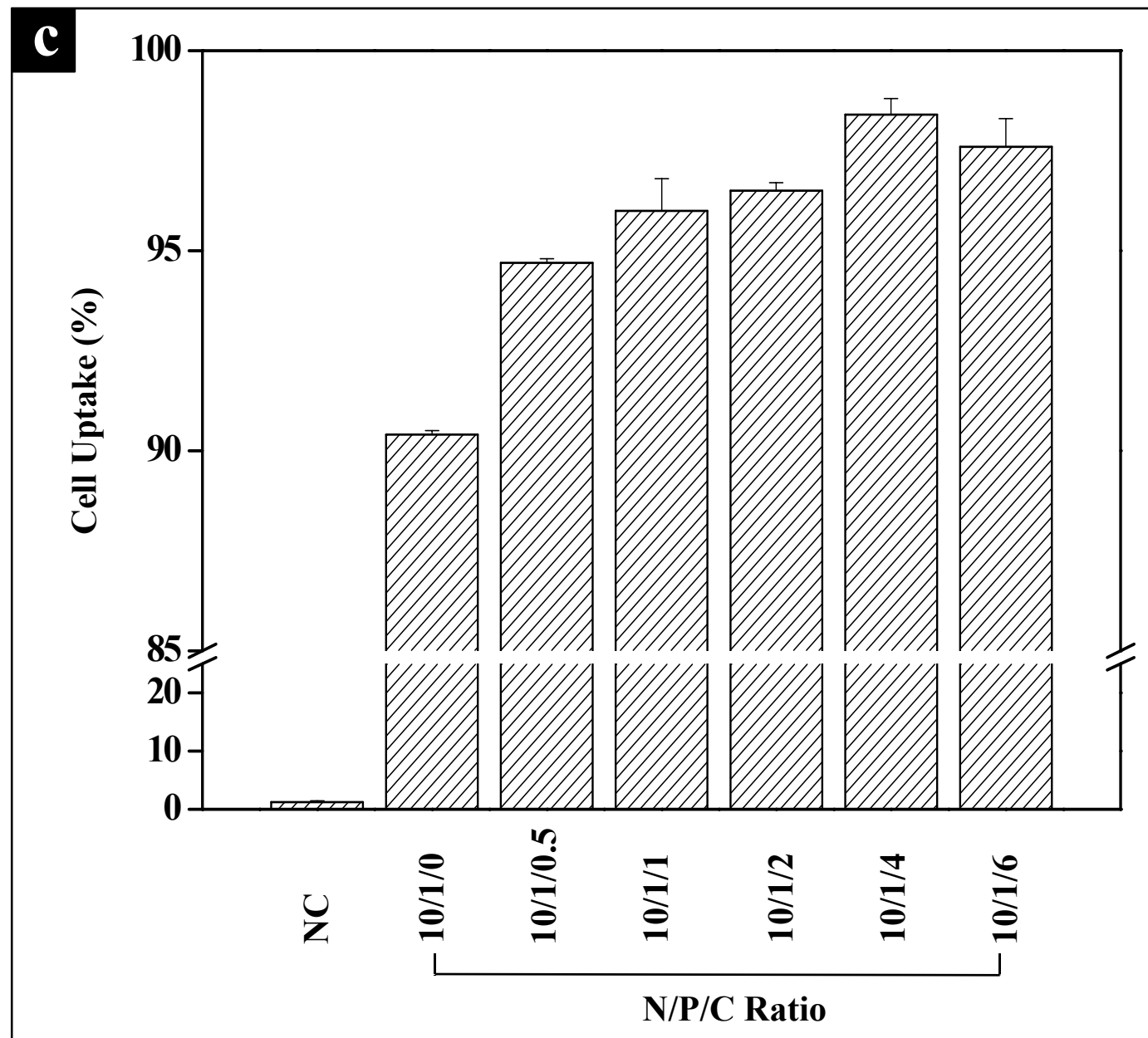


Figure 5

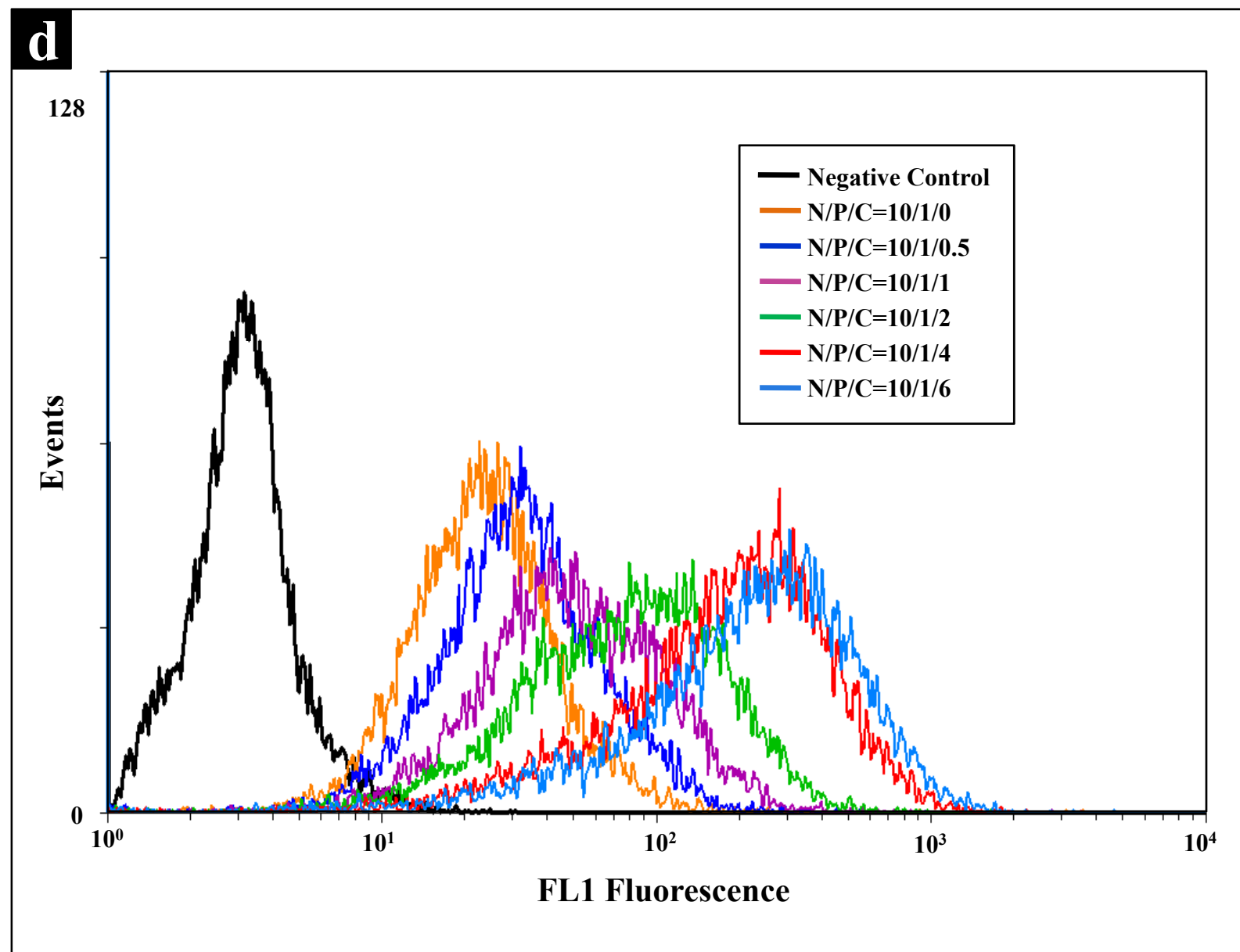


Figure 6

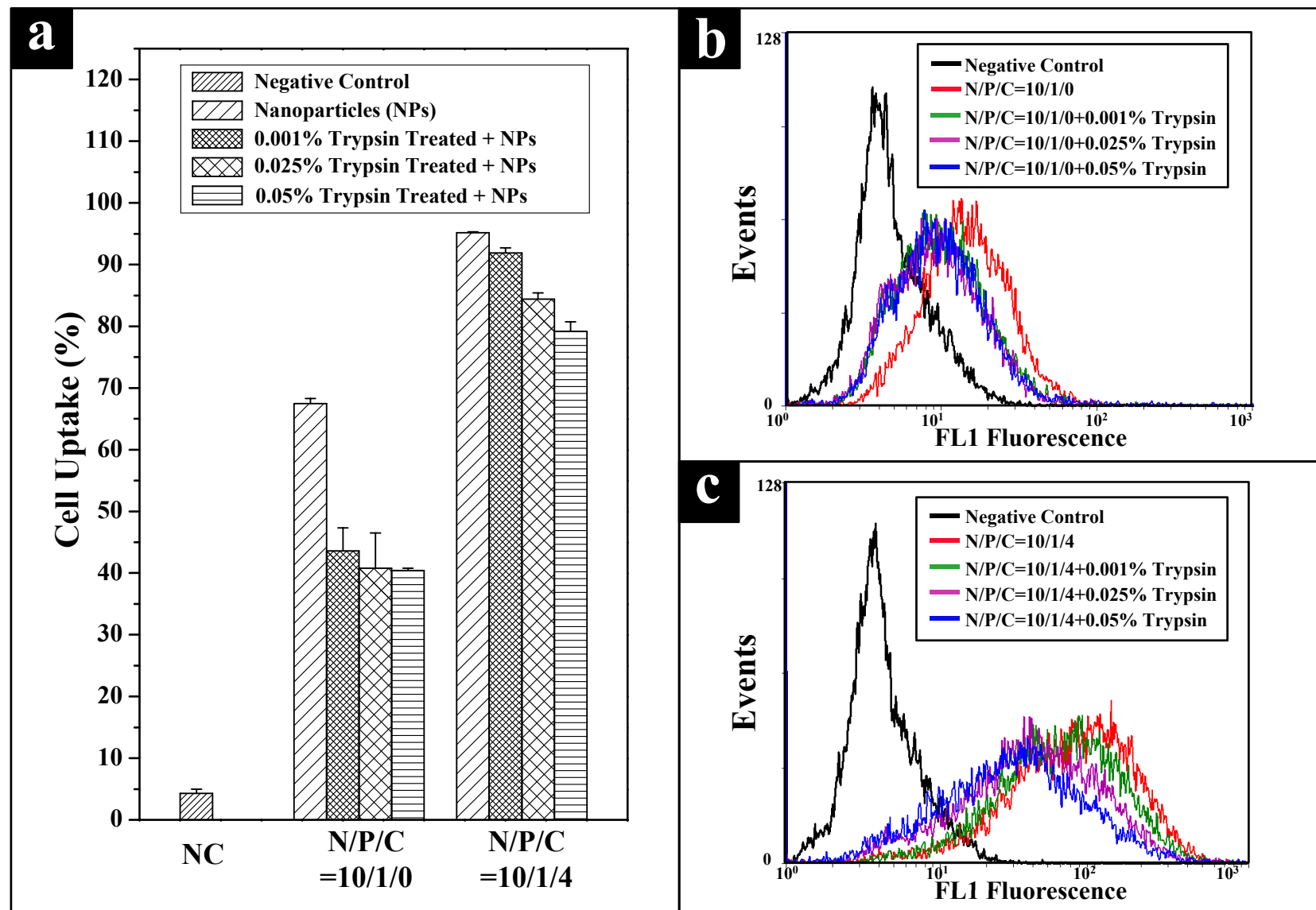


Figure 7

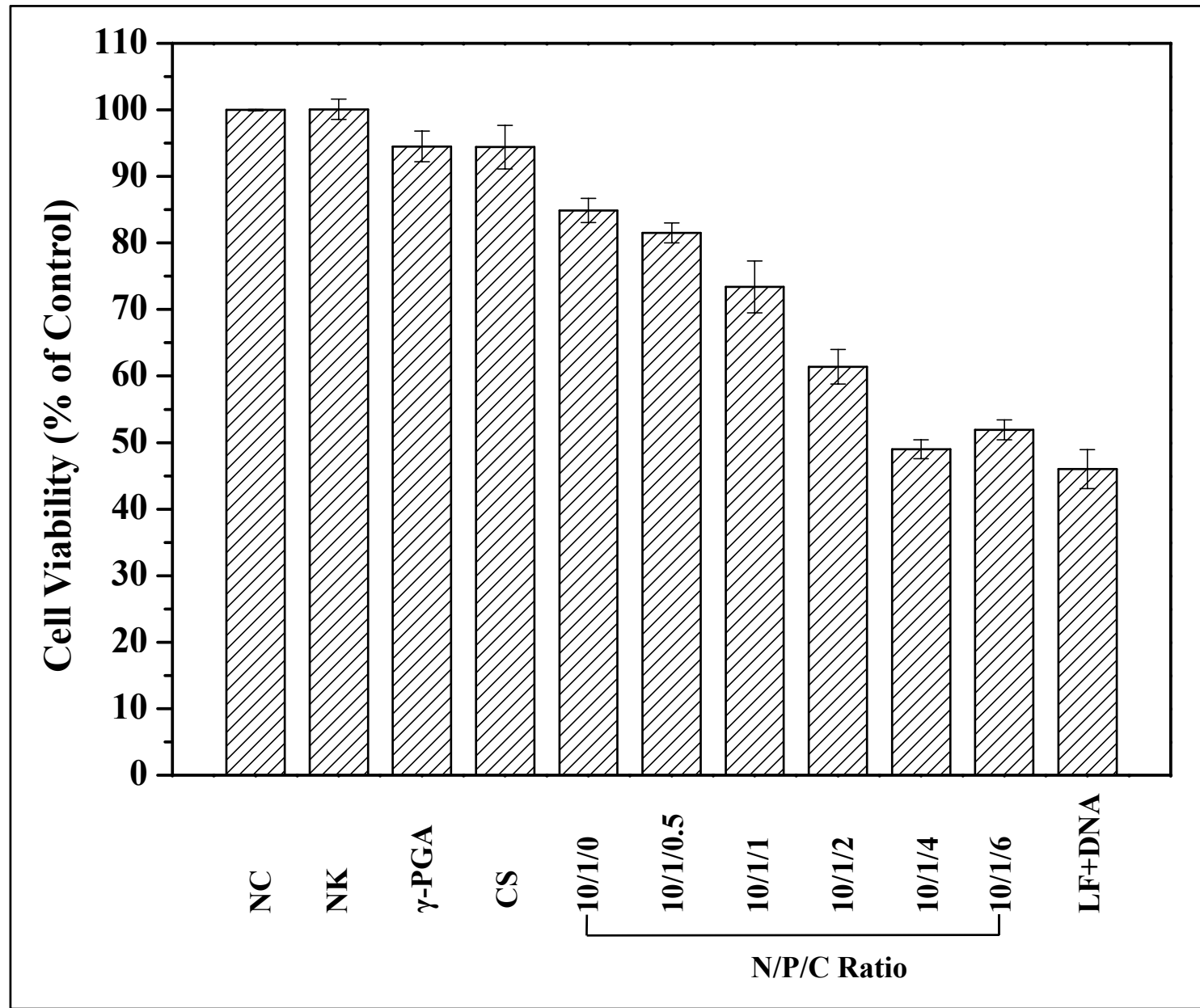




Figure 8

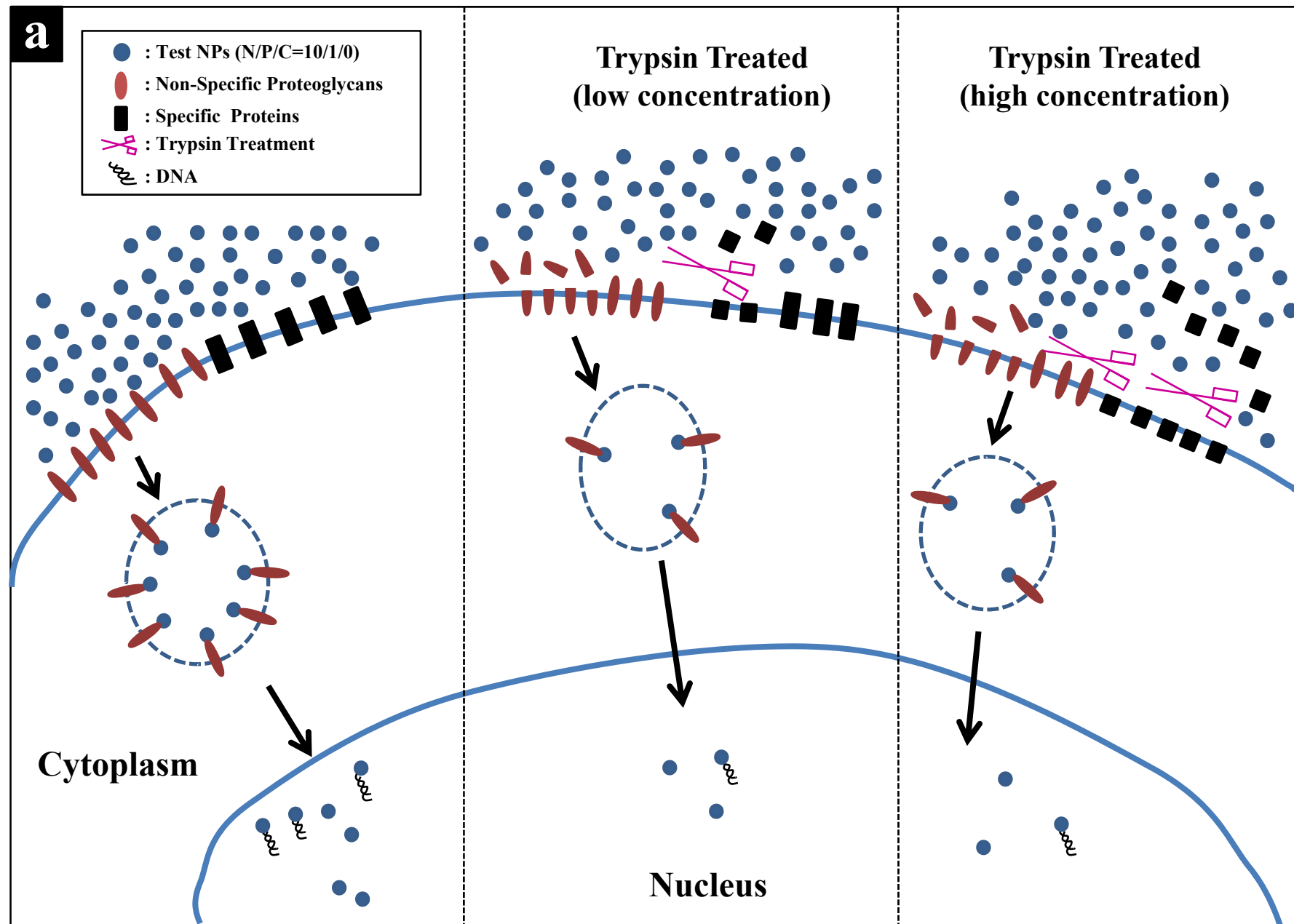


Figure 8

